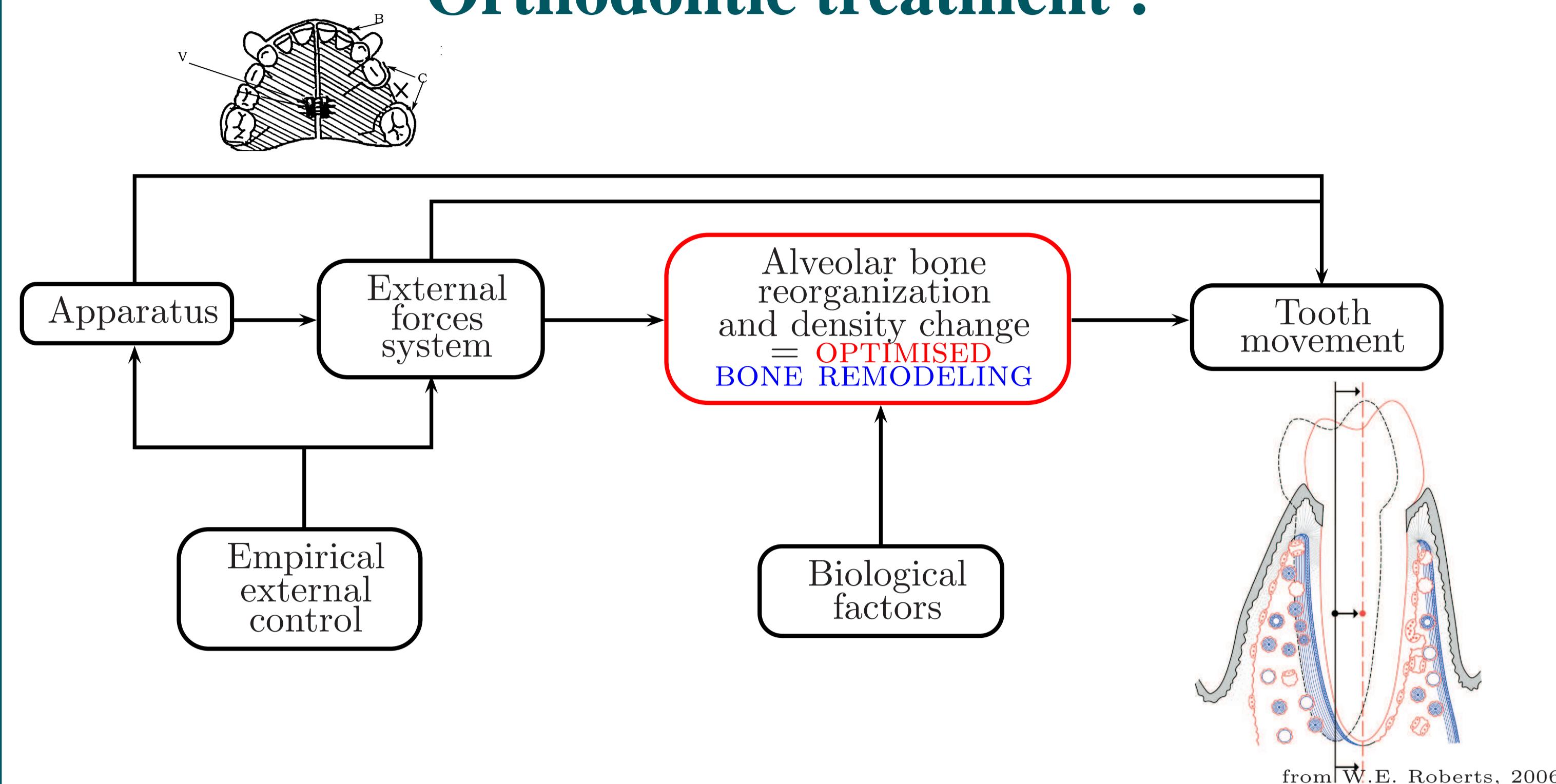


A continuum damage mechanics based bone remodeling model in a finite strains framework.

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Orthodontic treatment :



Bone remodeling = optimized bone mechanical response.

BUT orthodontic treatment plans mainly based on empirical knowledge \neq optimized treatment (mathematically speaking).

Aim : get a contribution to a treatment model

\Rightarrow model bone remodeling on a macroscopic scale
(phenomenological model)

Hypothesis : trabeculae mechanical behavior : elasto-plasticity
bone fibers alignment : orientation given by fabric tensor
bone density adaptation : $\dot{\rho} = kS_v \dot{r} \rho_0$

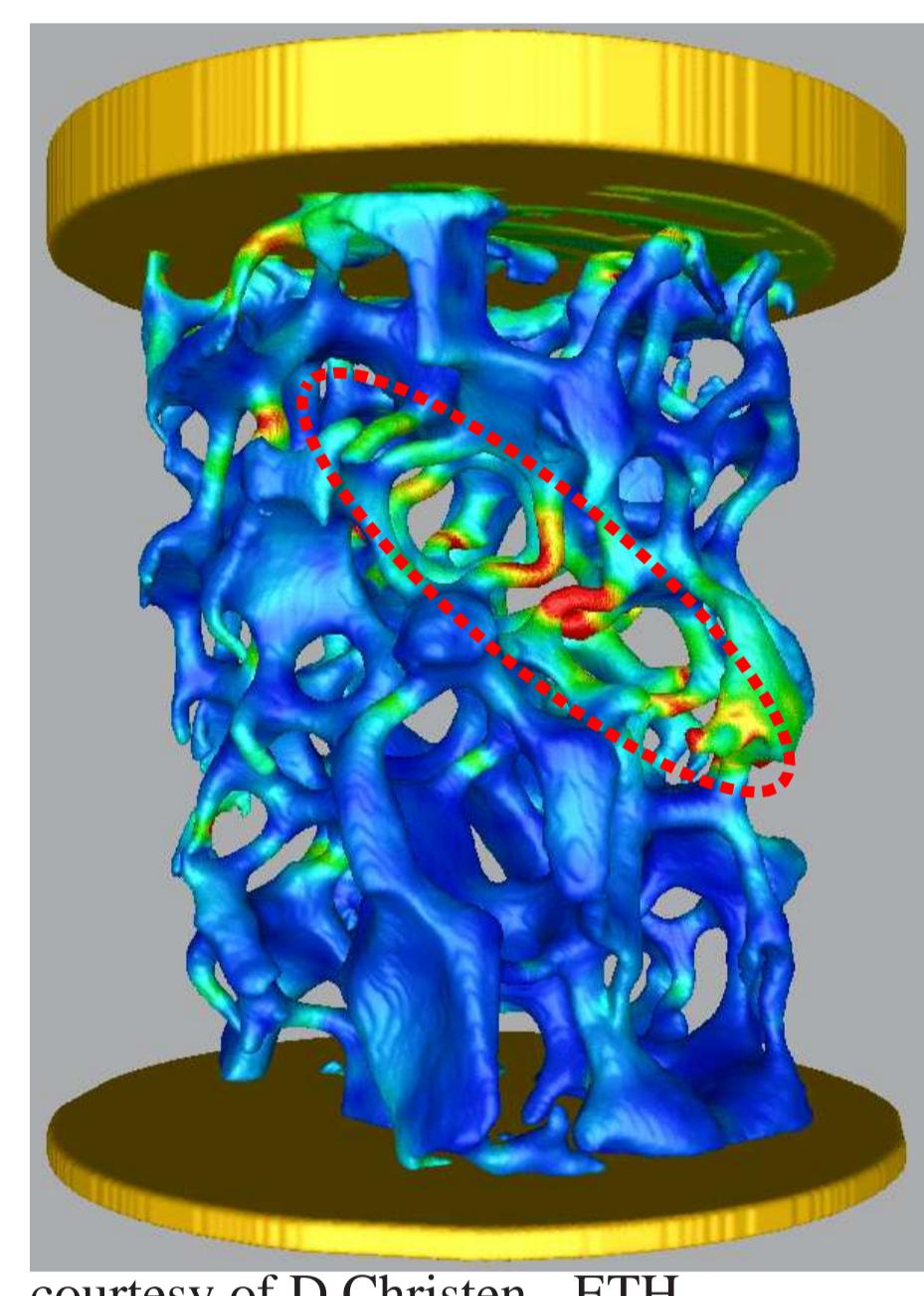
Mechanical **framework** : finite strains
continuum damage formulation

(no actual damage of the trabeculae) [1, 2]
finite element simulation (using Metafor [3])

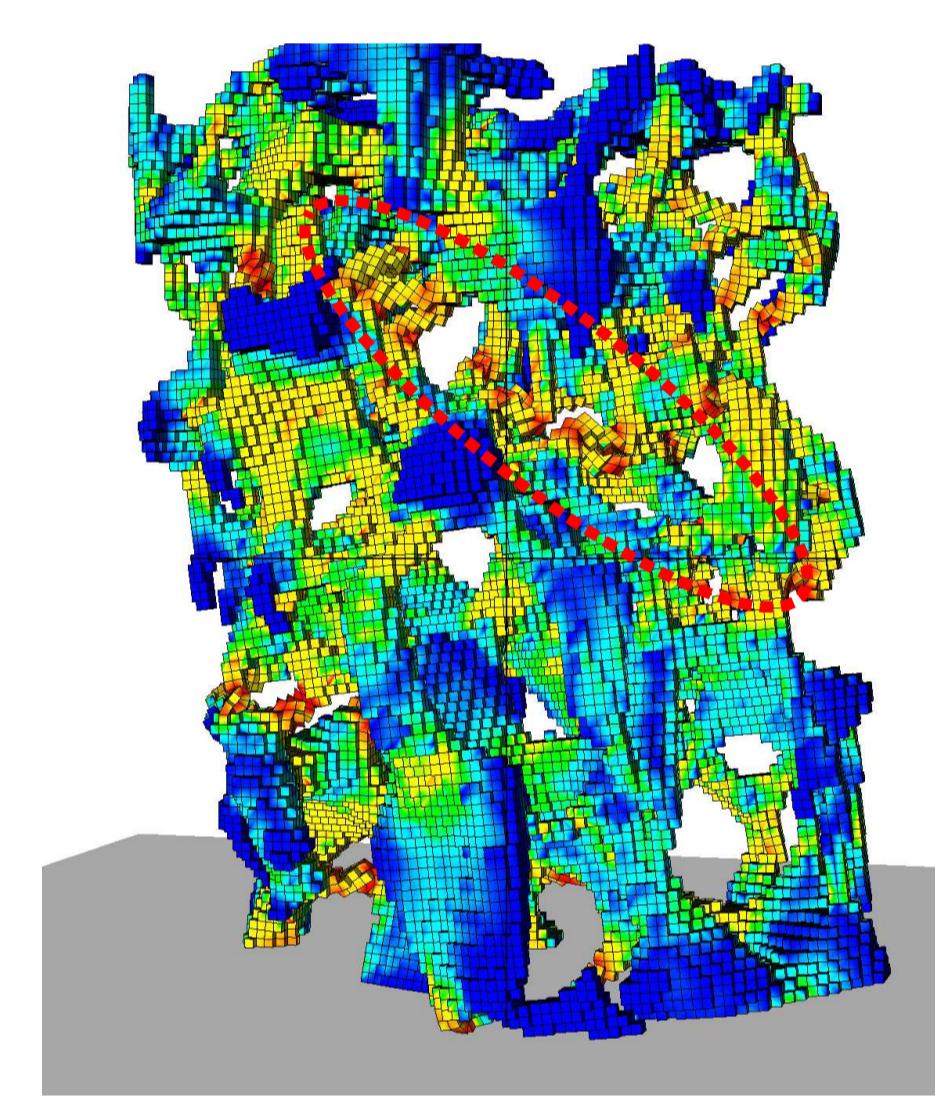
Testing the hypothesis :

Aluminium foam compression tests - non linear simulation / exp. data

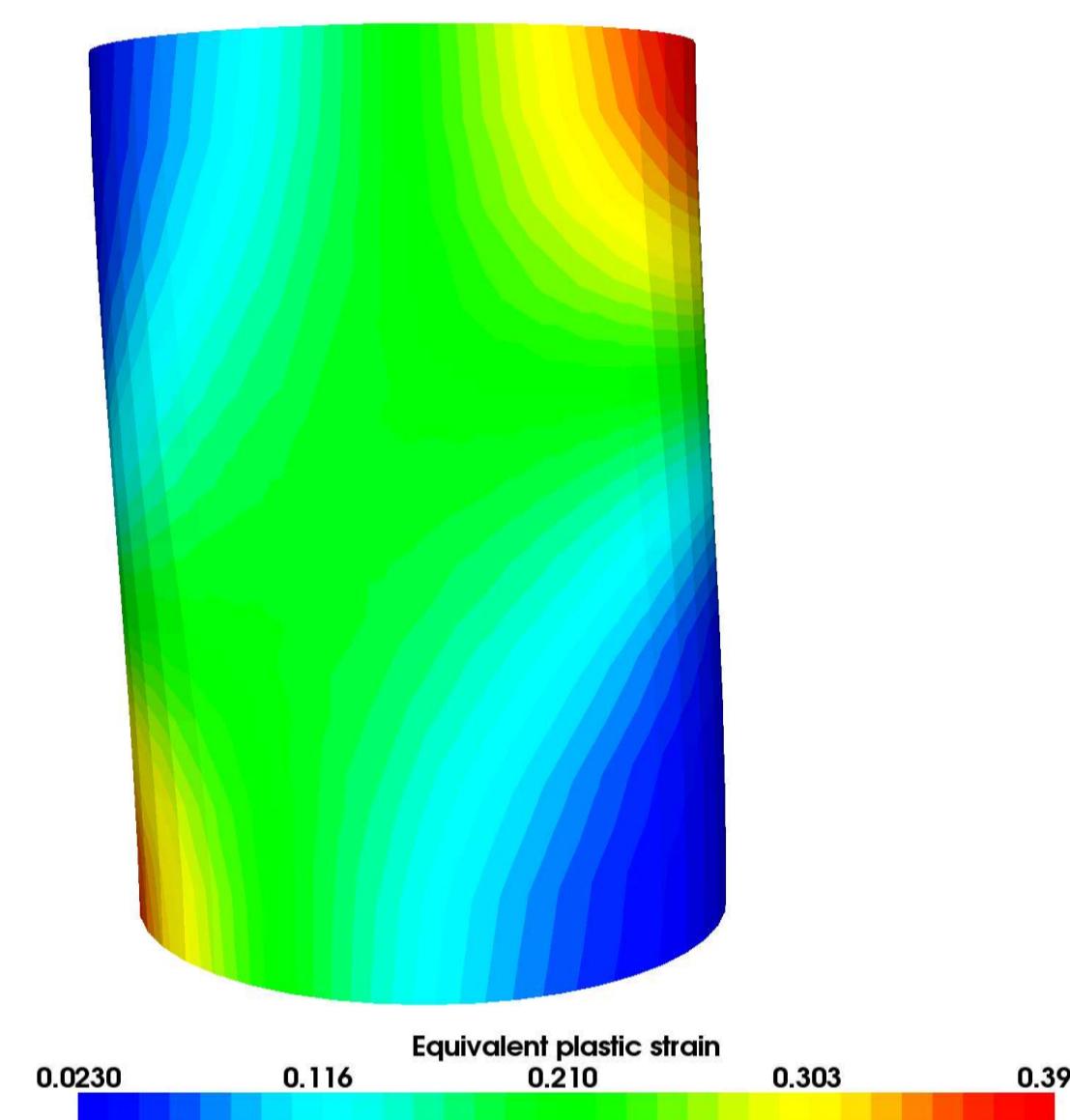
Exp. Data



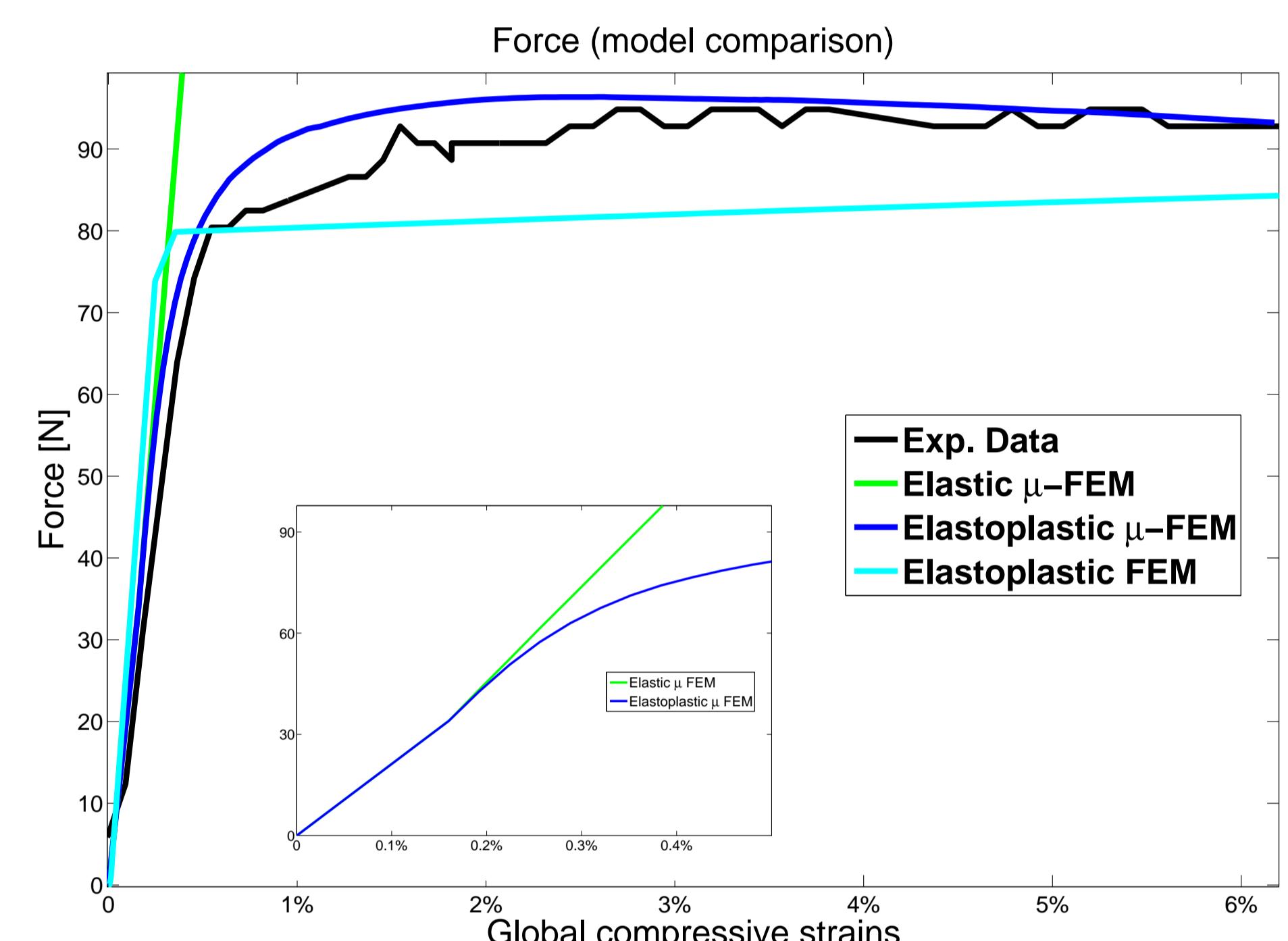
μ -FEM geometry from CT-scans



FEM fabric and apparent density derived from morphology data



Work done in collaboration with ETH - Institute of Biomechanics
Simulation results acquired after abstract submission.



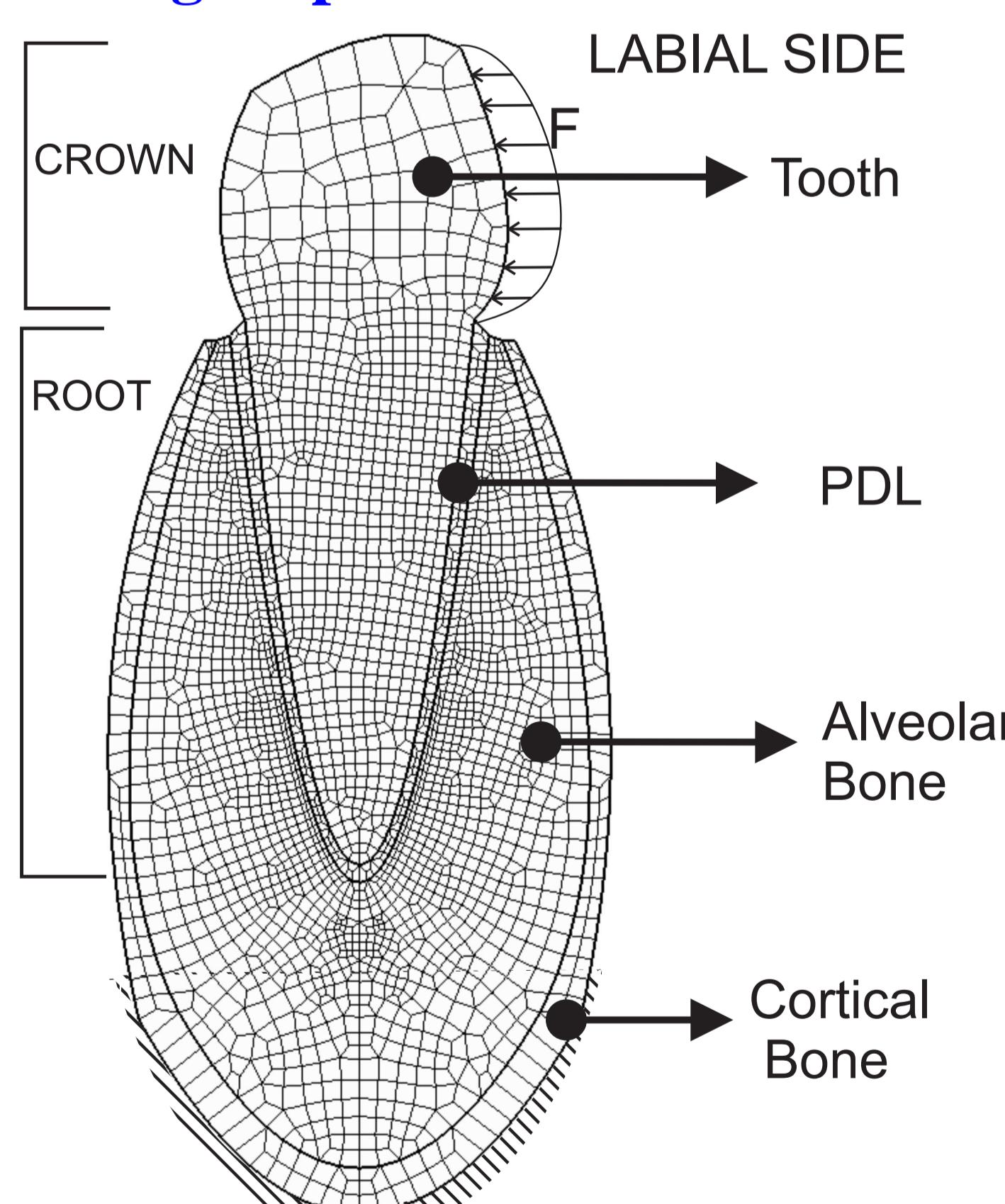
Both the overall deformation pattern and localization of high strains areas are well accounted for in the μ -FEM simulation. Highest strains appear to be on a plane where the apparent density is low. Significant differences between elastic and elasto-plastic simulations appear from 0.4% global compressive strains.

The use of a fabric tensor, homogeneous on the all Al. foam cylinder, allows to represent the overall sample deformation and the external force. It is not enough to represent failure plane. Fabric tensor models can therefore be used only on smaller representative volumes.

Preliminary results on remodeling :

Orthodontic treatment simulation : 2D idealized tooth

buccolingual plane

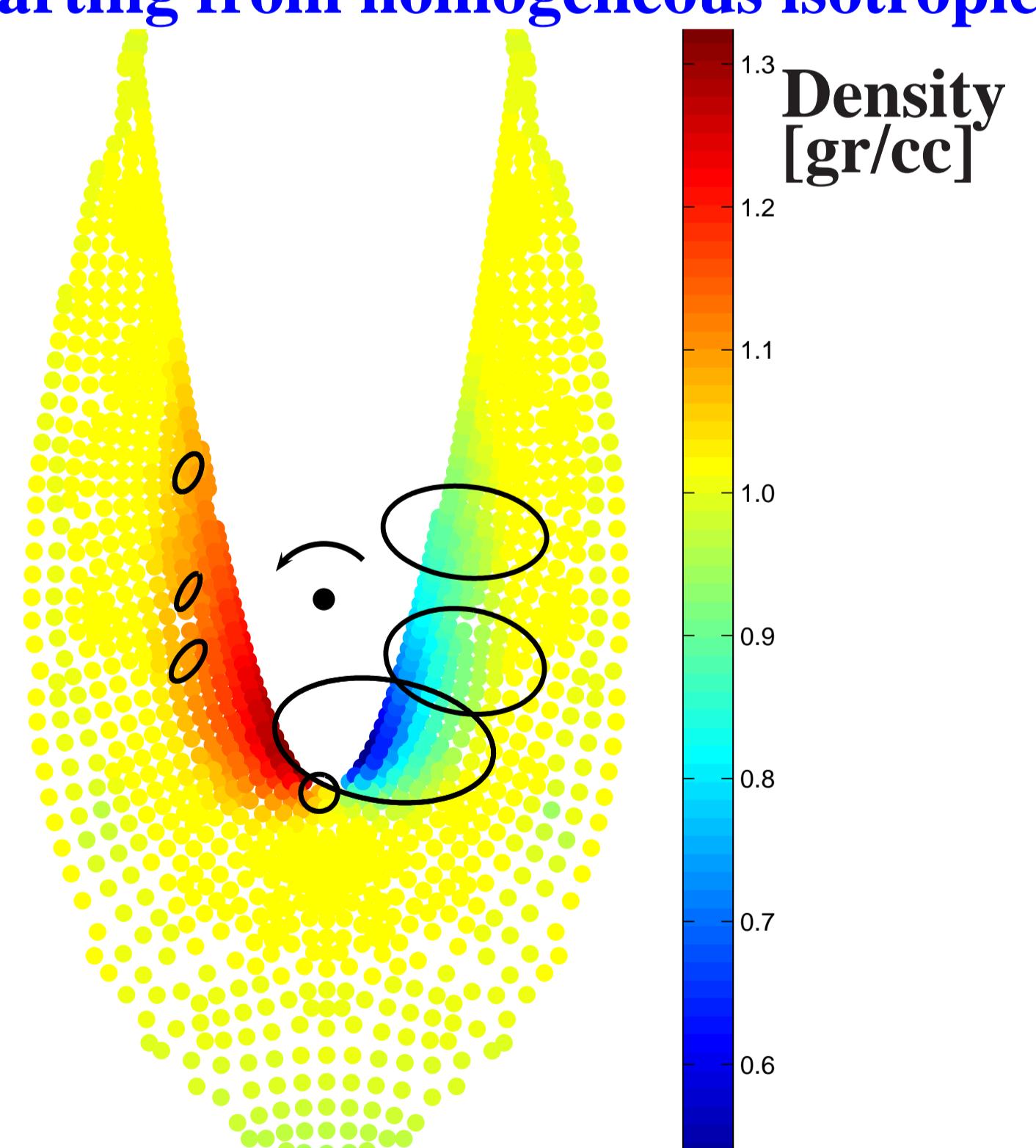


- Idealized 2D geometry : parabolic root plane strain state
- Linear elastic tooth and PDL
- Fabric-related elasto-plastic alveolar and cortical bone
- No gingiva
- Boundary conditions : constrained basal bone
labial pressure force on the crown
 \equiv orthodontic loading, tipping
(buccolingual rotation)

Results :

- Resorption and formation occur to allow tooth migration
(simulation can represent in-vivo behavior)
- Trabecular orientation aligns so that bone fibers are perpendicular to the tooth root surface, except at the apex where the pressure switches from tension to compression

remodeling after 3 weeks of constant loading starting from homogeneous isotropic bone



Ellipses show fabric principal directions, axis lengths inversely proportional to density
Plain circle and arrow show the center and direction of rotation

Ongoing/Future work :

Non linear behavior : validation

Validation of the FE analysis for 5 different samples, 3 densities (15 samples total).

Mesh convergence : use of at least 3 mesh resolutions

BC's representation : comparison of constrained/contact BC's

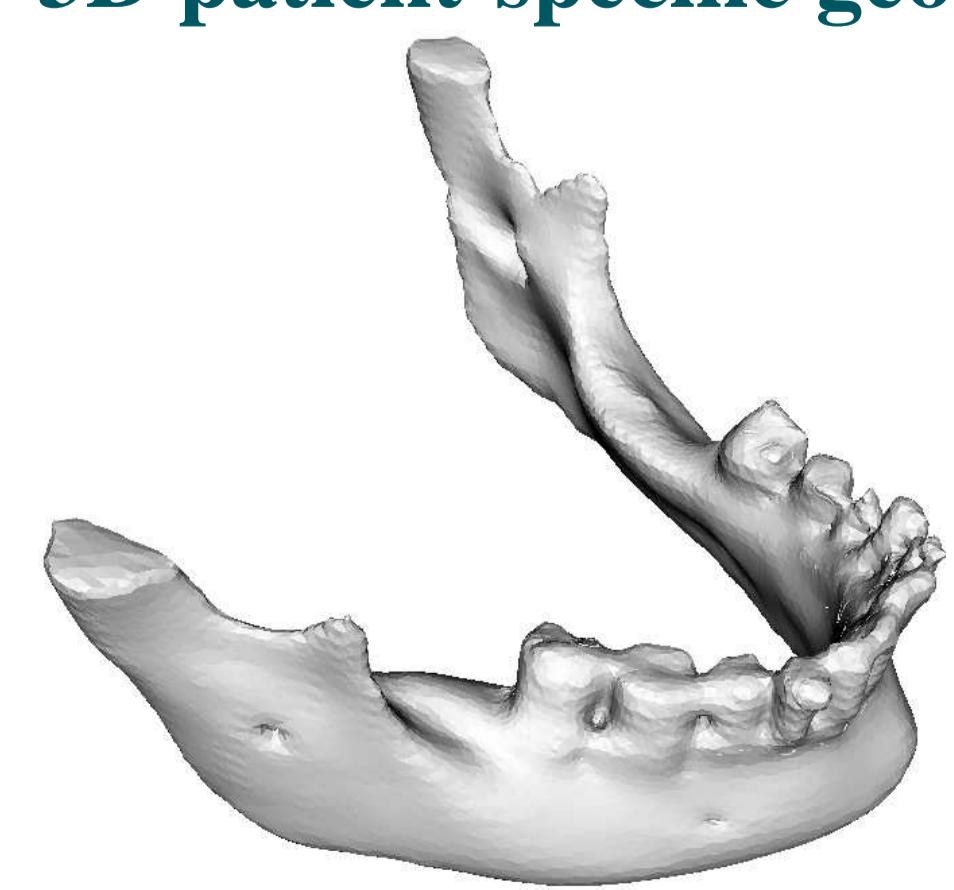
Type of integration : comparison of explicit, implicit and quasi-static FE analysis

Fabric/CDM formulation

Defining representative volumes for fabric.

Computing SED difference between continuum and μ -FEM (aim : no difference).

Orthodontic treatment simulation : 3D patient-specific geometry



Construction of patient-specific geometry (mesh from home-made triangulation mesher from CT-data)
Forces system from CAD-designed orthodontic appliances

Acknowledgment to

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Eidgenössische Technische Hochschule Zürich
Swiss Federal Institute of Technology Zurich

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