

MINERAL CONTENT AND BIOMECHANICAL PROPERTIES OF FIBROLAMELLAR BONE

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Hard Tissue I: Tissue Interactions

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Introduction



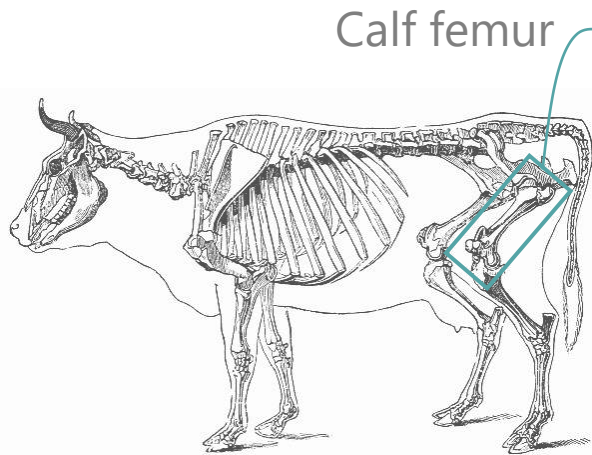
At birth: 30-40 kg  6-9 months: 220-320 kg  14-15 months: 550 kg

High stiffness, toughness, fracture resistance

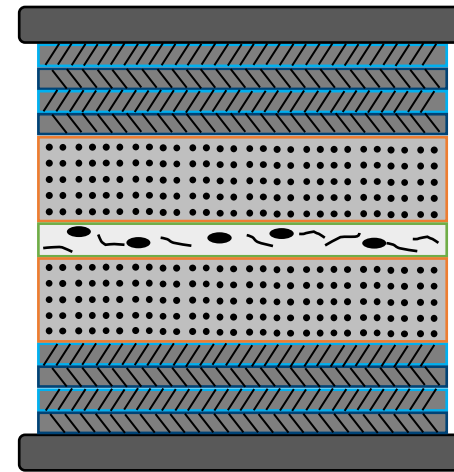
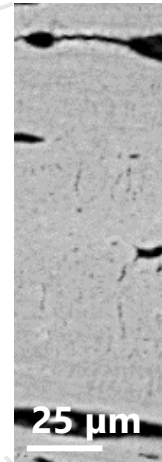
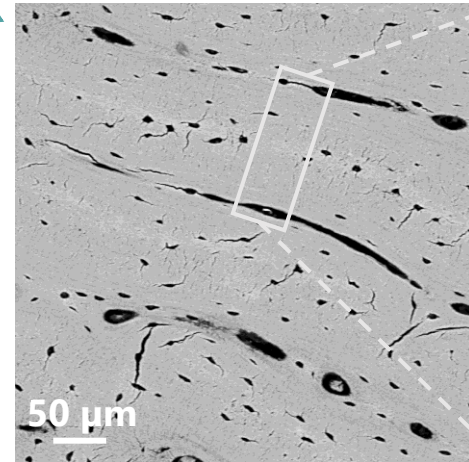


Fast growth

Introduction: fibrolamellar bone



<https://www.istockphoto.com>



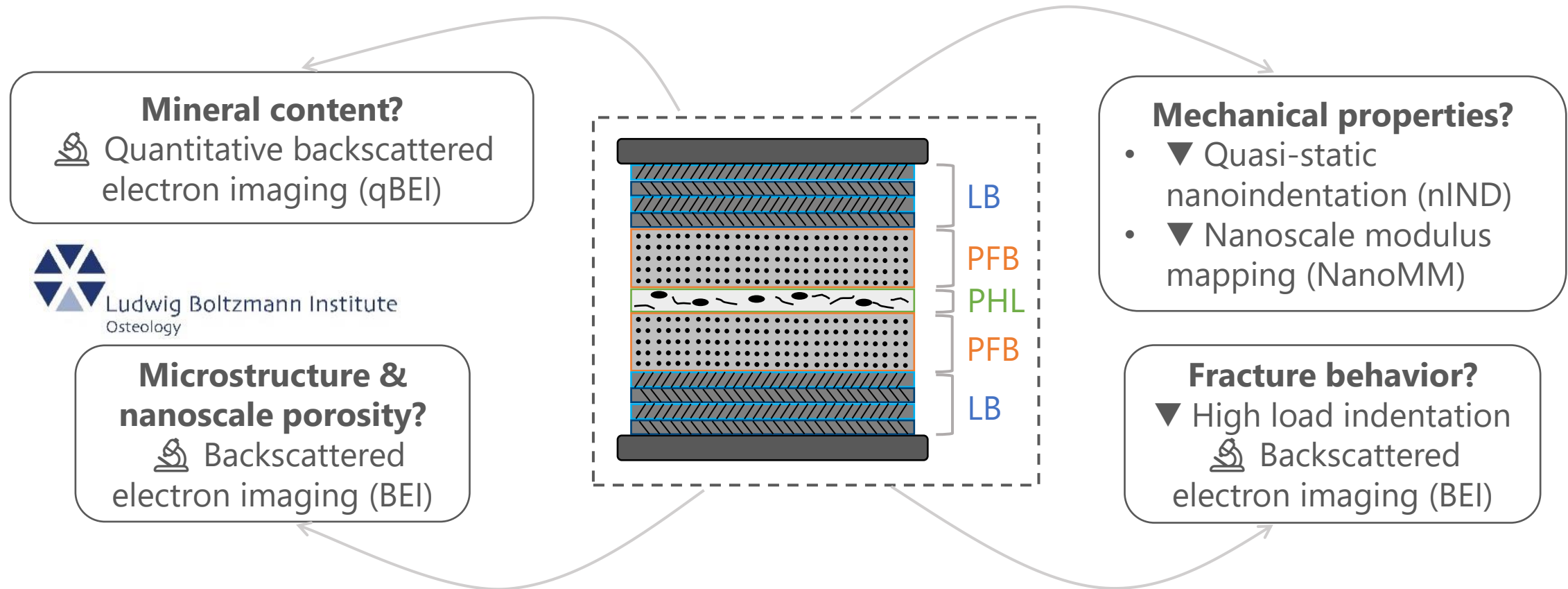
Blood vessel
 Lamellar bone (LB)
 Parallel-fibered bone (PFB)
 Primary hypercalcified layer (PHL)
 Parallel-fibered bone (PFB)
 Lamellar bone (LB)
 Blood vessel

- Microstructure (fibers orientation, cellular organization) ✓
- Apparent mechanical properties ✓
- Spatial distribution of mineral content ✗
- Local mechanical properties ✗

Clinical relevance: Similarity between deposition and callus formation in bone healing

Aims

Combination of imaging & mechanical testings to explore structure-function relationship

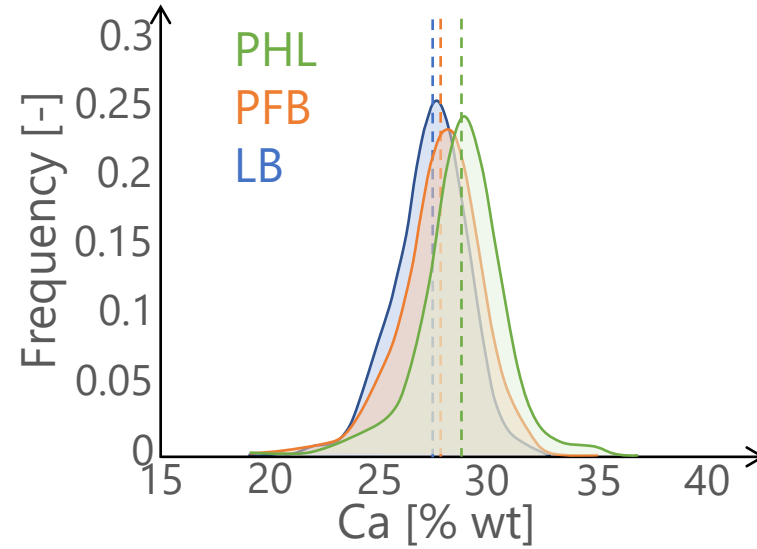
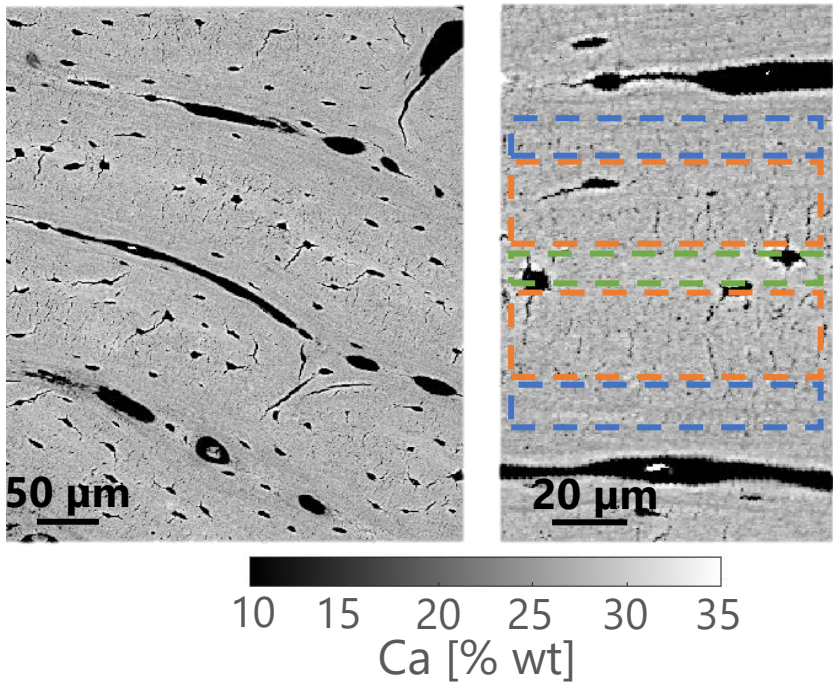


Mineral content, structure & nanoporosity

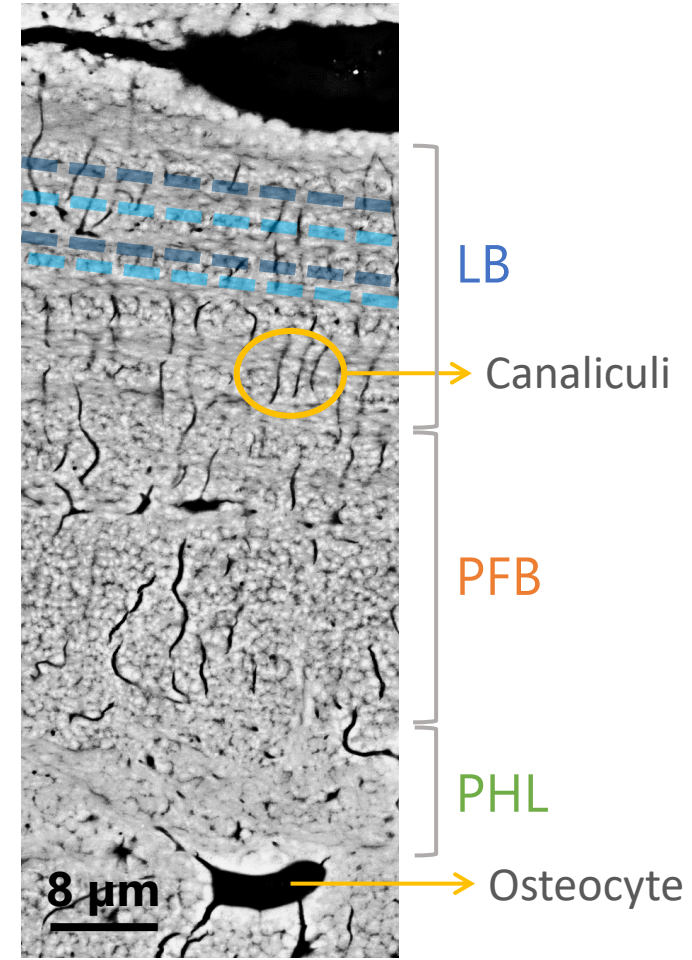
Quantification of local mineral content and visualization of microstructure & nanoscale porosity of fibrolamellar bone

 **BEI**
Resolution: 56 nm

 **qBEI**
Resolution: 0.57 μm



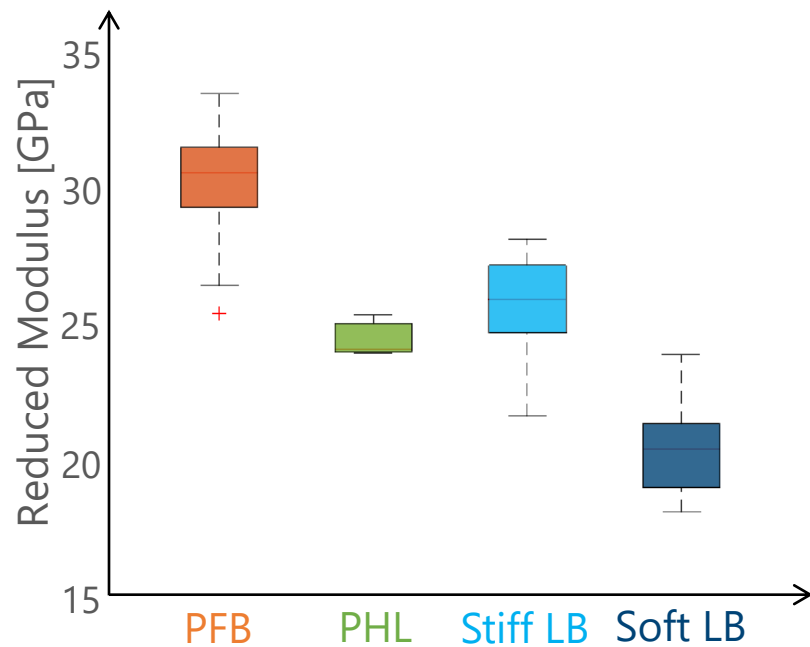
- PHL ~ 5% more mineralized
- LB made of alternating lamellae with \neq structures
- Osteocytes and less canaliculi in PHL



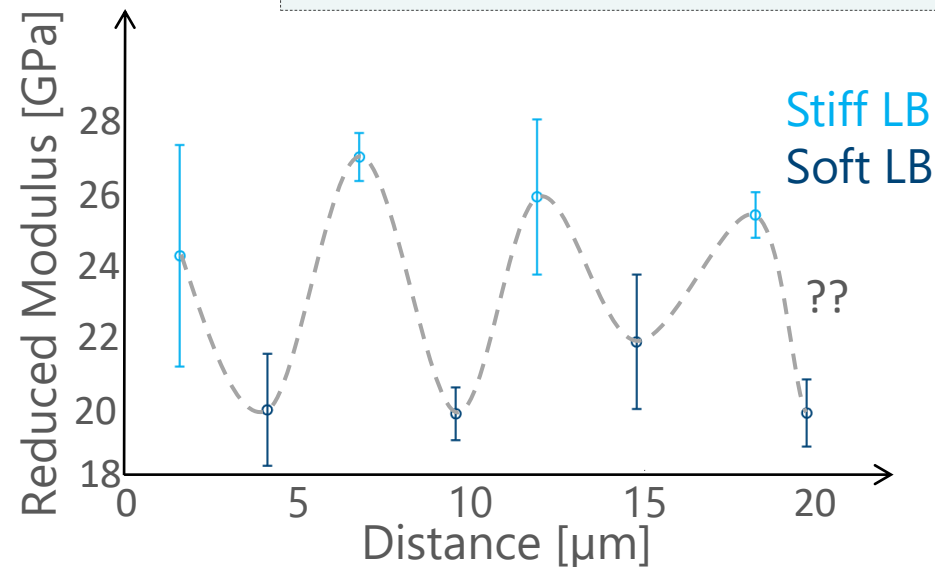
Mechanical properties with nanoindentation

▼ nIND

- Spacing: $\sim 6 \mu\text{m}$
- Applied force: $500 \mu\text{N}$
- Corresponding penetration depth: $\sim 150 \text{nm}$

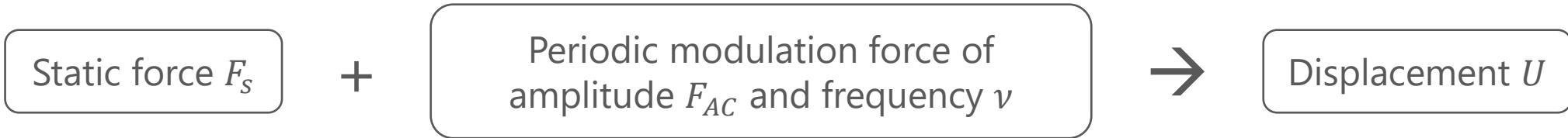


- PHL is softer than PFB
 - PFB is the stiffest region
 - Clear difference in mechanical behavior between lamellae
 - What about their transition?
- Need of **higher resolution** to characterize submicron mechanical behavior within LB

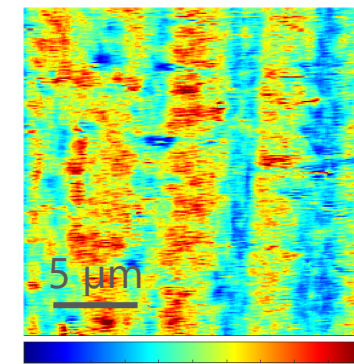
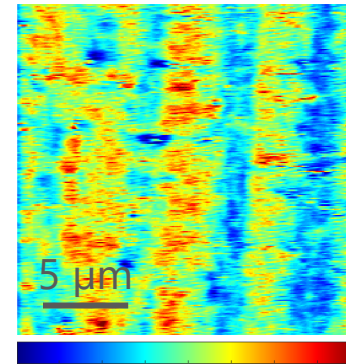
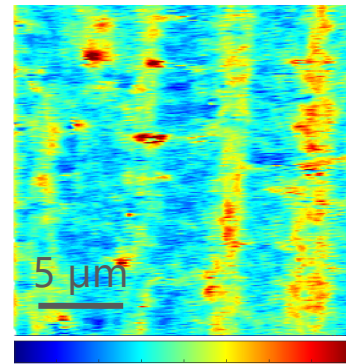
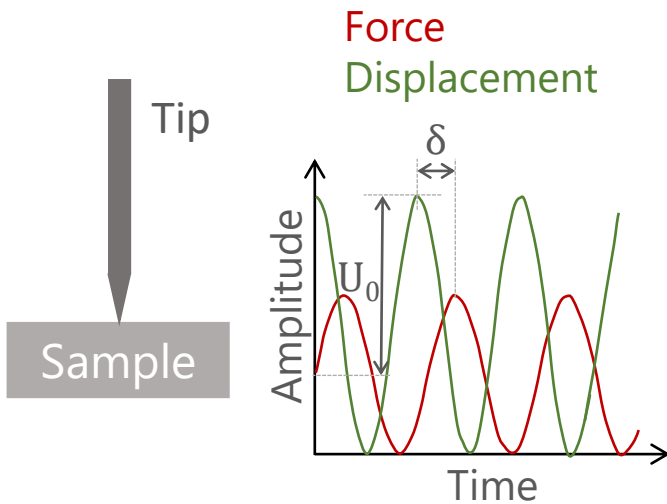


Modulus Mapping based on nanoindentation

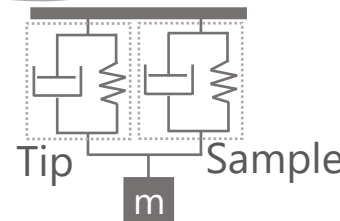
Nanoindentation combined with AFM-like piezo-scanner and force modulation system



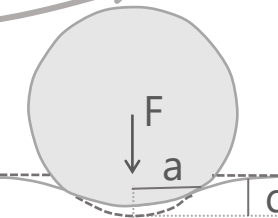
$$m\ddot{U} + C\dot{U} + KU = F_{AC}e^{i\omega t}$$



Kelvin-Voigt model assumption



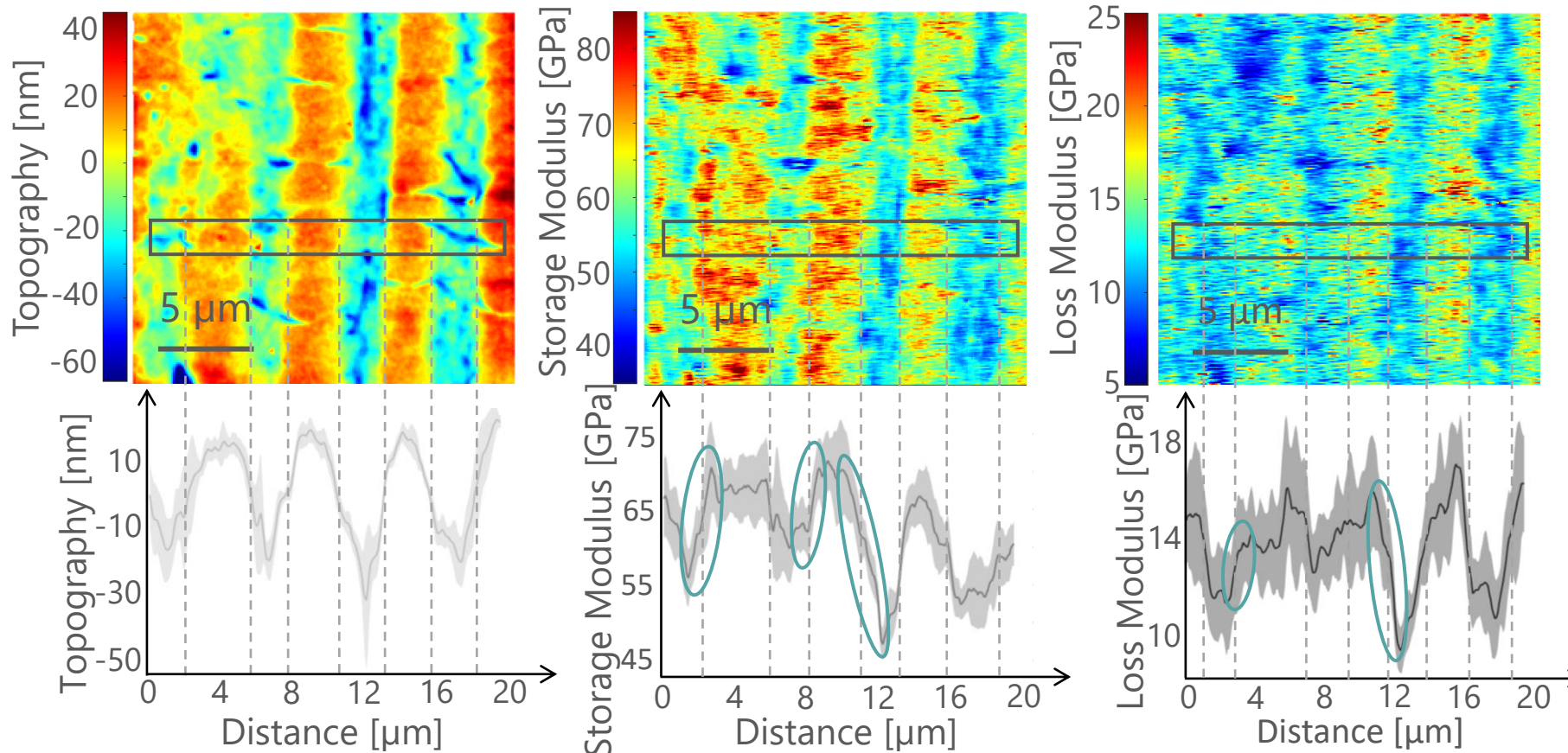
Hertz contact mechanics assumption



Mechanical properties with modulus mapping

▼ NanoMM

Static force: 3 μN | Dynamic force: 1 μN & 285 Hz | Penetration depth: ~ 6 nm | Lateral resolution: ~ 80 nm

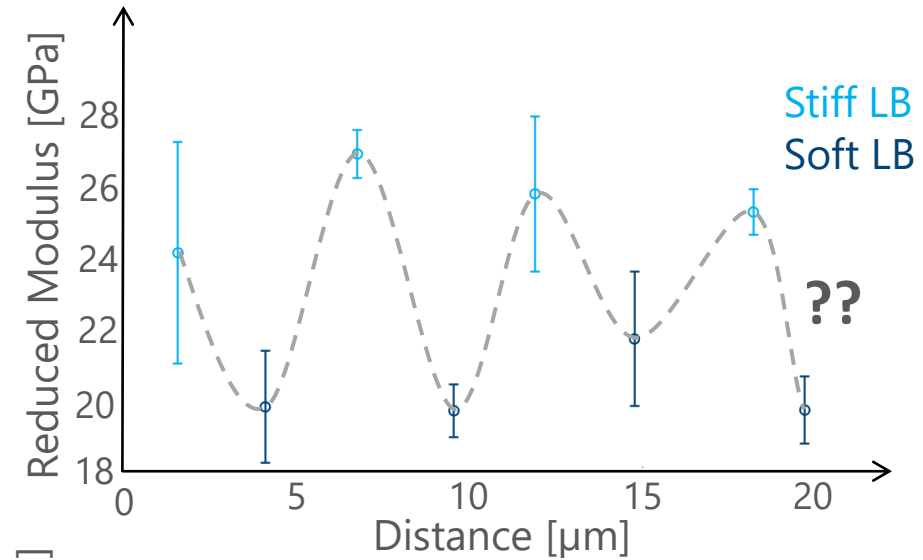


- Correlation with topography
- Alternating storage moduli
- Loss modulus with significant contribution
- **Steep** transition between lamellae: 0.8-1.4 μm

Two techniques, two length scales

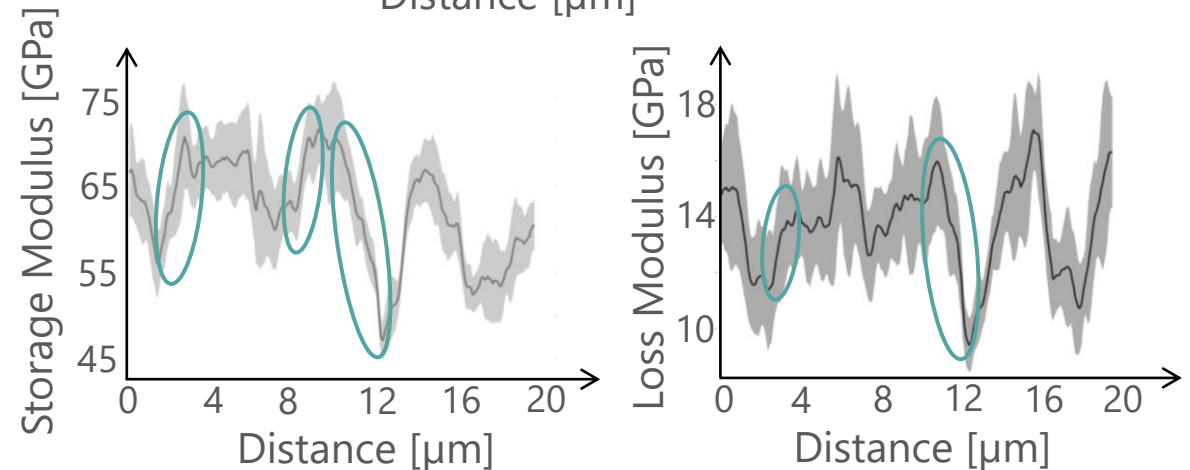
▼ nIND

- Large elastic field: 25X larger
- Probing pores & canaliculi
- ~**24%** difference between stiff and soft lamellae



▼ NanoMM

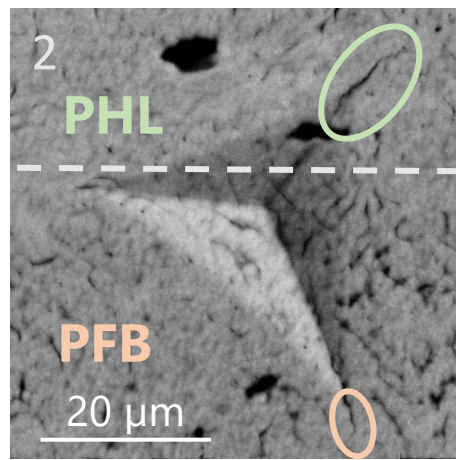
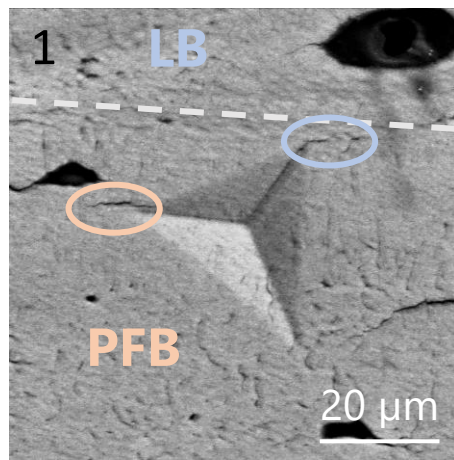
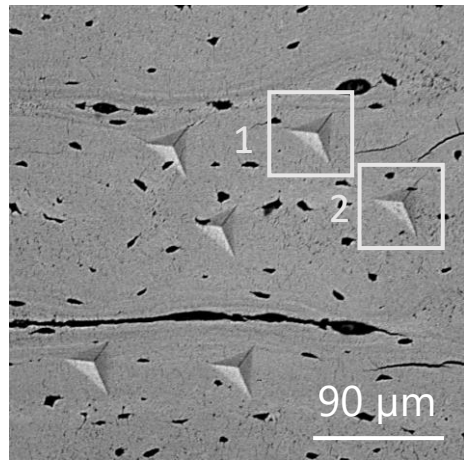
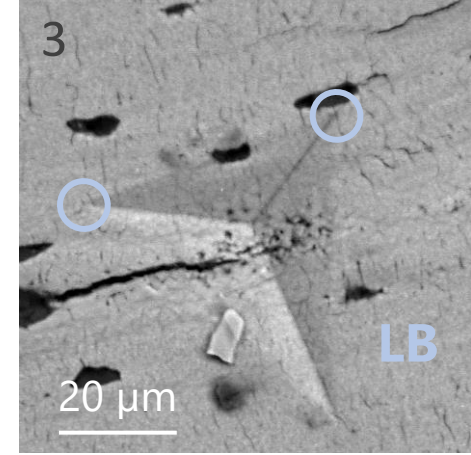
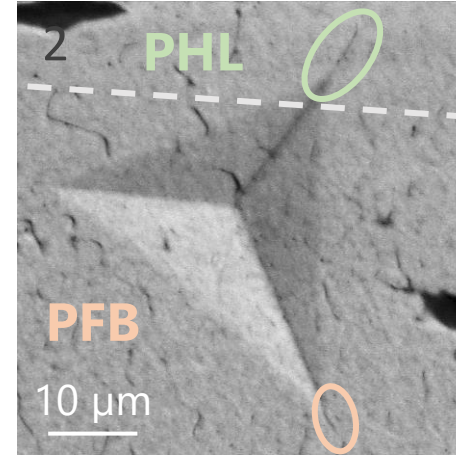
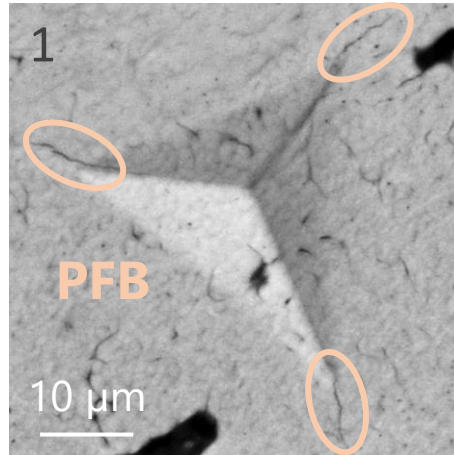
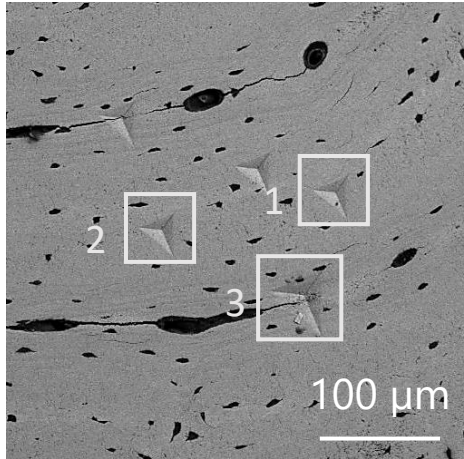
- Small elastic field: 25X lower
- Probing crystal-collagen composite on the surface
- ~**25%** difference between stiff and soft lamellae for storage & loss



Fracture behavior

Qualitative analysis of fracture behavior in each region

▼ High load indentation
Force applied: 0.5 N
BEI



- PFB: Straight cracks
- LB: Deflection at the interface & No cracks within region
- PHL: Longer cracks

Conclusion & Perspective

Mechanical and structural heterogeneity of fibrolamellar bone

Primary hypercalcified layer: Lower stiffness although higher mineral content and less porosity → Critical role of collagen organization

Parallel-fibered bone: **Stiffest** region

Lamellar bone: **Very sharp** modulation of elastic properties
→ Known to hamper crack propagation [Fratzl, Adv. Mater., 2007]

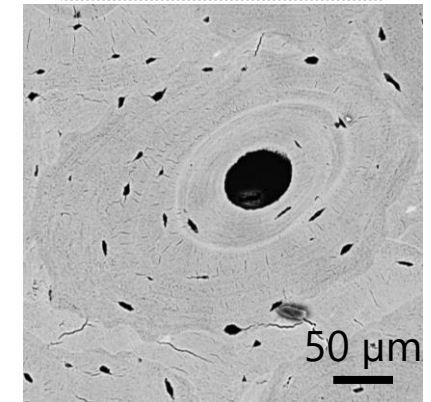
NanoMM technique is ideal to characterize small features/**interfaces** such as lamellae or cement lines (1-5 μm)

Fibrolamellar bone



Fast growth

High stiffness

High toughness



Thanks to all co-authors!

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Astrid
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Pauline
MURARO



Davide
RUFFONI



Markus
HARTMANN



Yann
DELAUNOIS



Philippe
COMPERE



Stéphane
BLOUIN



Thank you for your attention!



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