IMPACT OF ADVERSARIAL EXAMPLES ON DEEP LEARNING MODELS FOR BIOMEDICAL IMAGE SEGMENTATION

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Adaptive Segmentation Mask Attack

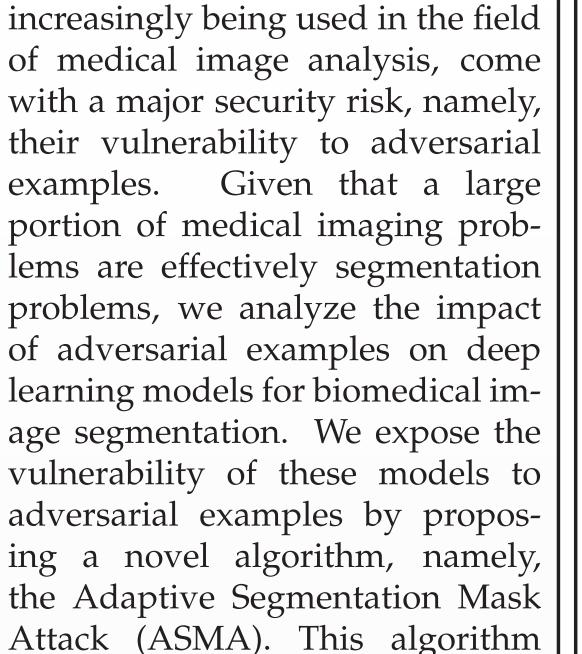
Genuine Image

Prediction: Cancer

Confidence: 0.95

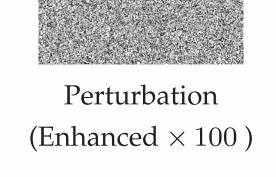
Adversarial examples are malicious data points that force machine learning models to make mistakes during testing time [2].

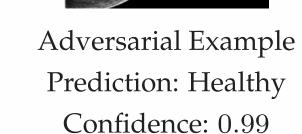
 $+ 0.01 \times$



Deep learning models, which are

By introducing a novel algorithm for producing targeted adversarial examples for image segmentation problems, we expose the vulnerability of deep learning models for biomedical image segmentation to malicious data points. Our algorithm, named Adaptive Segmentation Mask Attack (ASMA), incorporates two techniques, namely, the use of (1) adaptive segmentation masks and (2) dynamic perturbation multipliers. The proposed attack is defined







makes it possible to craft targeted adversarial examples that come with high Intersection-over-Union rates between the target adversarial mask and the prediction, as well as with perturbation that is mostly invisible to the bare eye.

Motivation

Abstract

Given that (1) labor expenses (i.e., salaries of nurses, doctors, and other relevant personnel) are a key driver of high costs in the medical field and (2) that increasingly super-human results are obtained by machine learning systems, an ongoing discussion is to replace or augment manual labor with *automation* for a number of medical diagnosis tasks [1]. However, a recent development called adversarial examples showed that deep learning models are vulnerable to gradient-based attacks [2]. This vulnerability, which is considered a major security flaw, for instance enables the creation of fraud schemes (e.g., for insurance claims) when deep learning models are carrying out clinical tasks [1].

as follows:

X : Input image.

 $g(\theta, \mathbf{X})$: Forward pass from a neural

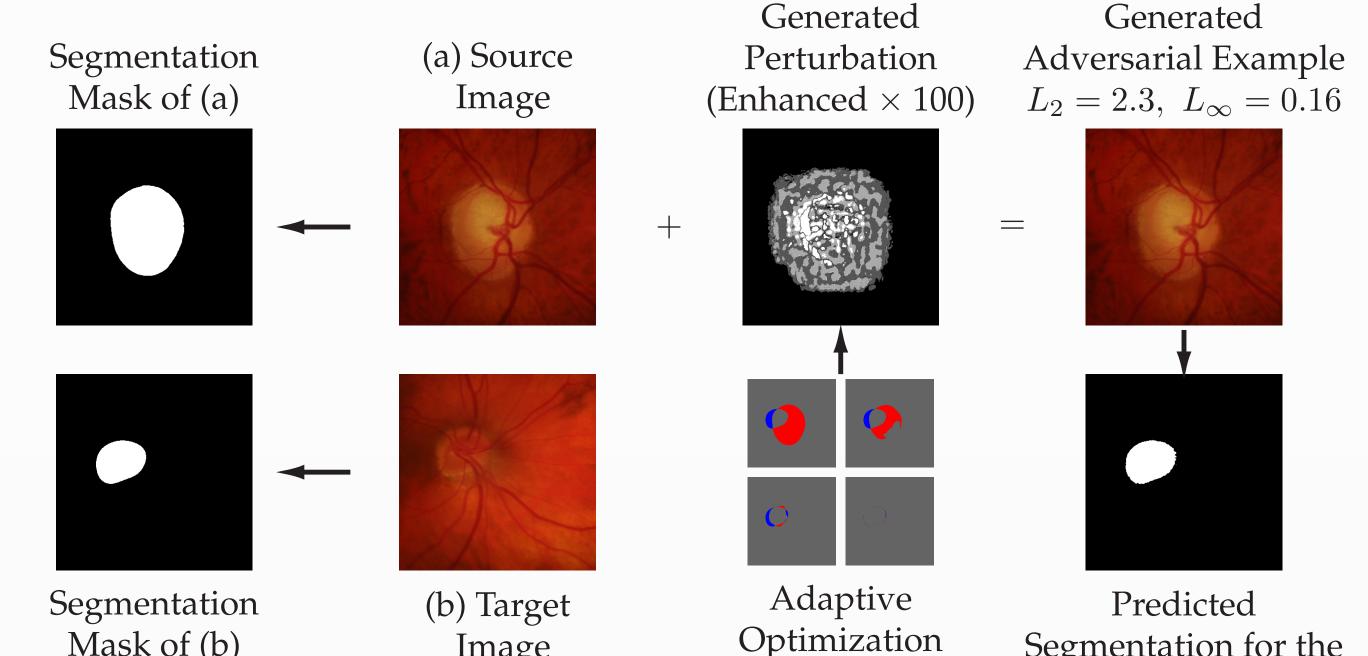
network *g* with parameters θ using input **X**.

- \mathbf{Y}^{A} : Target (adversarial) mask.
- \mathbf{P}_n : Added perturbation at *n*th iteration.

minimize $|| \mathbf{X} - (\mathbf{X} + \mathbf{P}) ||_2$,

such that $\arg \max \left(g(\theta, (\mathbf{X} + \mathbf{P})) \right) = \mathbf{Y}^A$, $(\mathbf{X} + \mathbf{P}) \in [0, 1]^z$, $\mathbf{P}_n = \sum_{c=0}^{n-1} \nabla_x \left(g(\theta, \mathbf{X}_n)_c \odot \mathbb{1}_{\{\mathbf{Y}^A = c\}} \odot \mathbb{1}_{\{\arg\max_M(g(\theta, \mathbf{X}_n)) \neq c\}} \right).$

ASMA is able to craft adversarial examples with 97% and 89% Intersection-over-Union (IoU) accuracy for the Glaucoma Dataset [3] and the ISIC Skin Lesion Dataset [4], respectively, with IoU measured between the predicted segmentation for a given adversarial example and the corresponding target mask. While doing so, our algorithm modifies the image so subtly that the perturbations, for the most part, are not visible to the bare eye.



The above observations motivate our effort to better understand the impact of adversarial examples on deep learning approaches towards biomedical image segmentation, so to facilitate the *secure* deployment of deep learning models during clinical tasks.

Mask of (b) (Target Mask)

Image

Segmentation for the Adversarial Example IoU = 98%, PA = 99%

Using ASMA, results obtained for the two above-mentioned biomedical datasets (mean and standard deviation) are provided in the table below (PA denotes Pixel Accuracy).

Masks

	Glaucoma Dataset				ISIC Skin Lesion Dataset			
	Modif	ication	Accu	iracy	Modification		Accuracy	
Optimization	L_2	L_{∞}	IoU	PA	L_2	L_{∞}	IoU	PA
ASMA	2.47	0.17	97 %	99%	3.88	0.16	89 %	98%
	± 1.05	± 0.09	$\pm 2\%$	$\pm 1\%$	± 1.99	± 0.09	$\pm 10\%$	$\pm 1\%$

The experiments presented above are conducted in white-box settings, using the U-Net architecture [5].

References		
 Finlayson S.G., Chung H.W., Kohane, I.S., Beam A.L., <i>Adversarial Attacks Against Medical Deep Learning Systems</i> Szegedy C., Zaremba W., Sutskever I., Bruna J., Erhan D., Goodfellow I., Fergus R., <i>Intriguing Properties of Neural Networks</i> Pena-Betancor C., Gonzalez-Hernandez M., Fumero-Batista F., Sigut J., Medina-Mesa E., Alayon S., de la Rosa M., 		
 Estimation of the Relative Amount of Hemoglobin in the Cup and Neuroretinal Rim using Stereoscopic Color Fundus Images [4] Gutman D., Codella N., Celebi M., Helba B., Marchetti M., Mishra N., Halpern A., Skin Lesion Analysis toward Melanoma Detection [5] Ronneberger O., Fischer P., Brox T., U-Net: Convolutional Networks for Biomedical Image Segmentation 	GHENT UNIVERSITY	Center for Biotech Data Science