

# Electrophysiological correlates of behavioural changes in vigilance in vegetative state and minimally conscious state

Eric Landsness,<sup>1,2,\*</sup> Marie-Aurélie Bruno,<sup>1,\*</sup> Quentin Noirhomme,<sup>1</sup> Brady Riedner,<sup>2</sup> Olivia Gosseries,<sup>1</sup> Caroline Schnakers,<sup>1</sup> Marcello Massimini,<sup>3</sup> Steven Laureys,<sup>1</sup> Giulio Tononi<sup>2</sup> and Mélanie Boly<sup>1</sup>

- 1 Coma Science Group, Cyclotron Research Centre and Neurology Department, University of Liège and Centre Hospitalier Universitaire du Sart-Tilman, Liège, Belgium
- 2 Department of Psychiatry, University of Wisconsin Madison, Madison, WI, USA
- 3 Department of Clinical Sciences, 'Luigi Sacco', University of Milan, Milan, Italy

Correspondence to: Giulio Tononi, Department of Psychiatry, University of Wisconsin–Madison, 6001 Research Park Blvd, Madison, WI 53719, USA

E-mail: gtononi@wisc.edu

Correspondence may also be addressed to: Mélanie Boly, Cyclotron Research Centre, Allee du 6 Aout, 8, B30, 4000 Liege, Belgium E-mail: mboly@student.ulg.ac.be

The existence of normal sleep in patients in a vegetative state is still a matter of debate. Previous electrophysiological sleep studies in patients with disorders of consciousness did not differentiate patients in a vegetative state from patients in a minimally conscious state. Using high-density electroencephalographic sleep recordings, 11 patients with disorders of consciousness (six in a minimally conscious state, five in a vegetative state) were studied to correlate the electrophysiological changes associated with sleep to behavioural changes in vigilance (sustained eye closure and muscle inactivity). All minimally conscious patients showed clear electroencephalographic changes associated with decreases in behavioural vigilance. In the five minimally conscious patients showing sustained behavioural sleep periods, we identified several electrophysiological characteristics typical of normal sleep. In particular, all minimally conscious patients showed an alternating non-rapid eye movement/ rapid eye movement sleep pattern and a homoeostatic decline of electroencephalographic slow wave activity through the night. In contrast, for most patients in a vegetative state, while preserved behavioural sleep was observed, the electroencephalographic patterns remained virtually unchanged during periods with the eyes closed compared to periods of behavioural wakefulness (eyes open and muscle activity). No slow wave sleep or rapid eye movement sleep stages could be identified and no homoeostatic regulation of sleep-related slow wave activity was observed over the night-time period. In conclusion, we observed behavioural, but no electrophysiological, sleep wake patterns in patients in a vegetative state, while there were near-to-normal patterns of sleep in patients in a minimally conscious state. These results shed light on the relationship between sleep electrophysiology and the level of consciousness in severely brain-damaged patients. We suggest that the study of sleep and

<sup>\*</sup>These authors contributed equally to this work.

homoeostatic regulation of slow wave activity may provide a complementary tool for the assessment of brain function in minimally conscious state and vegetative state patients.

Keywords: sleep; vegetative state; minimally conscious state; consciousness; EEG

Abbreviations: REM = rapid eye movement

# Introduction

Traditionally, coma is clinically defined by a state of total lack of arousal and behavioural unresponsiveness. When patients in comas start to open their eyes and show a behavioural sleepwake cycle (extended periods of eye closure and muscle inactivity), they usually evolve towards a vegetative state, which can be transient or persistent. Vegetative state is defined by periods of preserved behavioural arousal (eyes open with decreased arousal threshold), but an absence in signs of self-awareness or the environment (Laureys and Boly, 2007, 2008). Patients in a minimally conscious state additionally show non-reflexive or purposeful behaviours, but are unable to communicate effectively (Giacino et al., 2002). Clinically, the differential diagnosis between these two patient populations is extremely challenging, leading to a high rate of misdiagnosis in the absence of a proper clinical scale (Schnakers et al., 2009). Several studies have however shown important differences in brain function (Boly et al., 2008a; Vanhaudenhuyse et al., 2010) and prognosis (Laureys and Boly, 2007; Luaute et al., 2010) between patients in vegetative or minimally conscious states.

Sleep is a universal phenomenon that is present in all animal species and throughout life (Cirelli and Tononi, 2008). In addition to behavioural decreases in vigilance (assessed clinically by the closing of eyes and muscle inactivity), mammalian sleep has a number of highly reliable electrophysiological features such as slow waves, spindles and rapid eye movements (REMs). The sequential alternation of sleep stages, the presence of sleep cycles and the homoeostatic regulation of slow waves are characteristics of sleep that are found universally in healthy human volunteers (Dijk et al., 1993; Riedner et al., 2007). The presence of standard sleep elements could also reflect global brain integrity as they have been shown to be altered in several pathological states such as stroke (Bassetti and Aldrich, 2001; Gottselig et al., 2002) and Alzheimer's disease (Crowley et al., 2005).

There remains a debate about the presence of sleep electrophysiological correlates to changes in behavioural vigilance observed in patients in vegetative or minimally conscious states (Bekinschtein et al., 2009a; Cologan et al., 2010). Indeed, behavioural fluctuations in arousal are classically related mainly to brainstem and basal forebrain function, i.e. to a differential activity of the ascending reticular activating system (Boly et al., 2008b). Consequently, closing of the eyes and inactivity does not necessarily imply related changes in thalamocortical function, which would more likely be reflected by detectable scalp EEG changes, particularly in patients presenting widespread thalamocortical disconnections (Vanhaudenhuyse et al., 2010). Previous studies have suggested that patients in a vegetative state may show both preserved behavioural and electrophysiological sleep (Oksenberg et al., 2001; Isono et al., 2002). However, these studies did not explicitly differentiate patients in a vegetative state from patients in a minimally conscious state when assessing the patients' residual brain function. Furthermore, only a restricted set of sleep parameters were reported and therefore the interpretation of these findings in brain-damaged patients is limited. Hence, we performed sleep recordings in 11 patients with severe brain damage using high density EEG and investigated the presence of different stages of sleep, sleep cycle architecture and the regulation of homoeostatic slow-wave activity (the EEG power density between 0.5 and 4.5 Hz during non-REM sleep) in each individual patient. The use of high density EEG allowed us to maximize our chances of detecting electrophysiological features of sleep that correlate to changes in behavioural vigilance, despite the presence of extensive focal lesions commonly found in these patients. We hypothesized that the presence of normal sleep patterns, likely reflecting underlying functional brain integrity, could potentially differentiate patients in a vegetative state from those in a minimally conscious

# Materials and methods

#### **Patients**

We recorded nocturnal high-density EEG recordings in 11 brain-injured patients (six patients in a minimally conscious state, age 39  $\pm$  15 years (mean  $\pm$  standard error of the mean), range 19-55; five patients in a vegetative state, age  $54 \pm 18$  years, range 35-75). Further two patients were acquired but had to be excluded from our analyses due to excessive movement artefacts and ocular contamination of the recordings, resulting in poorly interpretable traces. Tables 1 and 2 report the demographic and clinical characteristics of the patients. Clinical examinations were performed repeatedly by trained neuropsychologists/assessors using the standardized Coma Recovery Scale-Revised (Giacino et al., 2004) and the Glasgow Liege Scale (Born, 1988) on the day of EEG recordings, in the week before and the week after. Patients were recorded in a non-sedated condition. The study was approved by the Ethics Committee of the Faculty of Medicine of the University of Liège and written informed consent was obtained from the patients' legal representatives.

# Data acquisition and analysis

In all subjects, 12 h recordings were acquired using a 256 electrode high-density EEG system (Electrical Geodesics) sampled at 500 Hz and referenced for acquisition purposes to Cz [the EEG acquisition system default setting; (Landsness et al., 2009)]. Recordings were performed from 8 a.m to 8 p.m; room lights were turned off at 10 p.m and

Table 1 Clinical, electrophysiological and structural imaging data of patients in a minimally conscious state

	MCS1	MCS2	MCS3	MCS4	MCS5	MCS6
Clinical Features Gender (age, years) Cause Days after insult Outcome at 12 months	F (22) Traumatic brain injury 2 years Glasgow Outcome Scale 3	M (46) Sub-arachnoïdal haemorrhage 1.5 year Glasgow Outcome Scale 3	F (45) Embolism, anoxia 5 years Glasgow Outcome Scale 3	M (46) Traumatic brain injury and cardiac arrest 25 years Glasgow Outcome Scale 3	M (19) Traumatic brain injury 7 months Glasgow Outcome Scale 3	M (55) Cardiac arrest 25 days Glasgow Outcome Scale
Breathing Paralysis/paresis Coma Recovery Scale -Revised Diagnosis Auditory function Visual function Motor function Communicate Arousal Total score	Tracheotomized Right paresis, left paralysis Minimally conscious state Auditory startle Visual pursuit Flexion withdrawal Vocalization/oral movement None Eyes open without stimulation	Spontaneous Right paresis, left paralysis Minimally conscious state Consistent movement to command Object recognition Automatic motor response Intelligible verbalization Non-functional Attention	Spontaneous Tetraparesis Minimally conscious state Localization to sound Visual pursuit Flexion withdrawal Vocalization/oral movement None Eyes open without stimulation	Spontaneous Tetraparesis Minimally conscious state Reproducible movement to command Visual pursuit Localization to noxious stimulation Vocalization/oral movement None Eyes open without stimulation	Spontaneous Tetraparesis Minimally conscious state Reproducible movement to command Visual pursuit Flexion withdrawal Wocalization/oral movement None Eyes open without stimulation	Spontaneous Tetraparesis Minimally conscious state Reproducible movement to command Object localization Localization to noxious stimulation Intelligible verbalization Non-functional intentional Attention
Medication Daily dosage	Phenobarbital 100 mg Baclofen 10 mg Scopolamine 1 patch	Levetiracetam 3*500 mg Valproic acid 3*287 mg Clonazepam 3*1 mg Esomeprazole 20 mg Perindopril 4 mg Amlodipine 10 mg Acetylcysteine 600 mg Bisoprol 10 mg	Baclofen 25 mg Cetirizine 10 mg Tramadol 25 mg Duloxetime 60 mg, Omeprazole 10 mg Domperidone 3*15 mg	Amantadine 200 mg Baclofen 2*10 mg Esomeprazole 20 mg Tizanidine 4 mg	Baclofen 3*15 mg Levetiracetam 3*500 mg Paracetamol 3*500 mg Caffeine 3*50 mg Atenolol 25 mg Enoxaparine 40 µg	Lorazepam 2.5 mg Esomeprazole 20 mg Clopidogrel 75 mg Acetylsalicylic acid 500 mg Simvastatine 40 mg Perindopril 4 mg Bisoprolol 2.5 mg Clanzapine 10 mg Enoxaparine 40 μg Glucophage 850 mg Amoxiclas 3*2 g Amoxiclas 3*2 g
EEG background activity MRI/CT	Fundamental rhythm: delta of low voltage Mesio-frontal and right brainstem lesions. Diffuse frontal and left cerebellum axonal injury. Diffuse cerebral atrophy.	Fundamental alpha rhythm with right and left lateralized theta Sub-arachnoidal hemorrhage due to aneurysm disruption, with lesions predominant in the left hemisphere.	desynchronized beta activity  Left frontal-temporal ischemic lesions; diffuse left cerebral and left cerebellar pedunde atrophy, bilateral periventricular white matter damage. Semioval centre and centro-	symmetrical theta activity  Quadri-ventricular hydrocephalus. Periventricular leucoence- phalopathy, bilateral fronto-parietal lesions. Diffuse cerebral atrophy, maximum in frontal and temporal lobes, hippo-	Fundamental delta rhythm and irregular theta activity.  Diffuse post traumatic axonopathy. Cerebellar and right middle peduncular lesions. Post traumatic micro hemorrhagic lesions in frontal lobes predominant on the right side.  Diffuse cerebral and	Theta activity  No detectable focal lesion.
			protuberantial sequellae.	campus, and thalami.	hippocampal atrophy.	

Table 2 Clinical, electrophysiological and structural imaging data of patients in a vegetative state

	VS1	VS2	VS3	VS4	VS5
Clinical features Gender (age, years) Cause Days after insult Outcome at 12 months	F (45) Hypoglycaemia 108days Glasgow Outcome Scale	F (70) Meningo-encephalitis 31days Glasgow Outcome Scale 3	F (75) Traumatic brain injury 38days Glasgow Outcome Scale 3	M (62) Pontine haemorrhage 49days Glasgow Outcome Scale 1	F (35) Anoxia 1 ½ year Glasgow Outcome Scale 2
Breathing Paralysis/paresis Coma Recovery Scale-Revised Diagnosis Auditory function	Tracheotomized Tetraparesis Vegetative state Auditory startle	Tracheotomized Tetraparesis Vegetative state Auditory startle Visual startle	Tracheotomized Tetraparesis Vegetative state Auditory startle	Tracheotomized Tetraparesis Vegetative state None	Tracheotomized Tetraparesis Vegetative state Auditory startle
Motor function Oromotor/Verbal function	Abnormal posturing Vocalization/oral movement	Flexion withdrawal Oral reflexive movement	None Oral reflexive movement	None	Flexion withdrawal Oral reflexive movement
Communicate Arousal Total score Medication	None Eyes open without stimulation 6	None Eyes open with stimulation 7	None Eyes open with stimulation 4	None Eyes open with stimulation 1	None Eyes open with stimulation 5
Daily dosage	Valproic acid 3* 287 mg Tetrazepam 3*25 mg Enoxoparine 40 μg	Lisinopril 10 mg Esomeprazole 20 mg Methylprednisolone 16 mg Furosemide 40 mg Amlodipine 5 mg	Amlodipine 5 mg Esomeprazole 40 mg Acetylsalicylic acid 100 mg Acetylcysteine 600 mg Enoxoparine 40 μg	Furosemide 2*40 mg Aldactazine 50 mg Acetylcysteine 600 mg Enoxoparine 40 µg	Levetiracetam 1000 mg Phenytoin 750 mg Valproate 4*650 mg Ranitidine 300 mg Aldactazine 50 mg Lorazepam 4 mg Levofloxacin 2*500 mg Paracetamol 4*1 g Vancomycin 1 g Enoxoparine 40 ug
EEG background Activity	Iso-electric	Symmetrical theta	Symmetrical theta	Irregular diffuse delta theta	Disorganized status epilepticus
MRIVCI	Diffuse white matter and basal ganglia lesions.	Frontal, temporal, periventricular, semi-oval centre, basal ganglia, thalamus and brainstem lesions.	Right temporal contusion & oedema. Bilateral frontal petechias. Left subdural hygroma.	Pontine, cerebellar peduncle and 4th ventricle haemorrhage.	No detectable focal lesion.

turned on again at 7.30 a.m. Video-taped recordings were acquired simultaneously and synchronously to the EEG data to confirm the patients' behaviour.

For each patient, sleep staging was based on EEG electrodes C3 and C4 referenced to mastoid electrodes A1 and A2 in accordance with Landsness et al. (2009). Sleep was scored in 20 s epochs according to standard schemes (Rechtschaffen and Kales, 1968). All EEG signals were down-sampled to 128 Hz and band-passed (two-way leastsquares finite impulse response) filtered between 0.5 and 45 Hz (35 Hz for one patient, due to abundant muscular artefacts). Electromyogram recordings were band-passed filtered between 5 and 40 Hz, whereas electro-oculogram recordings were filtered between 0.5 and 40 Hz.

As in previous studies (Riedner et al., 2007; Landsness et al., 2009), EEG power spectral analysis was performed on consecutive 4 s epochs (fast Fourier transform routine, Hanning window) using EEGLab (Delorme and Makeig, 2004). All artefacts were excluded both semi-automatically based on a threshold criteria and visually; then signals were average-referenced (Huber et al., 2004, 2006; Riedner et al., 2007; Landsness et al., 2009; Murphy et al., 2009, 2011; Kurth et al., 2010). For subjects in a minimally conscious state, we used 3.44  $\pm$  0.95 h of artefact free data (mean  $\pm$  standard error of the mean) and  $5.79 \pm 1.20$  for the patients in a vegetative state. Scalp topographies of non-REM slow-wave activity (0.5-4.5 Hz) were obtained averaging EEG power across all artefact-free epochs over the entire night (Figs 1 and 3). To compute differences in slow-wave activity between behavioural states, EEG power was averaged across all electrodes and compared using a paired t-test. While we have developed a sophisticated automatic algorithm for detecting spindles in healthy controls (Ferrarelli et al., 2010), it has not been validated in brain damaged patients. Given the challenges posed by data obtained from brain damaged patients, we chose to count spindles visually using the criteria of  $\sim$ 20–40  $\mu$ V activity with a waxing-waning appearance in the 12-16 Hz range with 0.5-2 s duration. Finally, in Figs 2 and 4, the homoeostatic decline of slow-wave activity is plotted over a single channel near Fz (Riedner et al., 2007). Values were obtained by averaging slow-wave activity power in each 20s window; then each segment of slow-wave activity was displayed sequentially over time. Subject-by-subject topographic changes in the homoeostatic decline in slow-wave activity were computed using statistical non-parametric mapping (simple threshold corrected P-value = 0.05 permutation test; Nichols and Holmes, 2002).

# **Results**

For patients in a minimally conscious state, behavioural sleep (sustained periods of eye closure and muscle inactivity) was accompanied by clearly detectable changes in EEG features, which looked similar to normal sleep (Fig. 1, left; Table 3). In the five patients in a minimally conscious state who showed consistent behavioural sleep over the night, we could detect periods corresponding to non-REM sleep (Stages 2-3) and periods of REM sleep, which occurred predominantly at the end of the night. In all minimally conscious state patients, we could also observe spindles during non-REM sleep. Within a given 30 min segment of data there was on average 16.3  $\pm$  8.0 spindles per patient (mean  $\pm$ standard error of the mean). Compared to periods of wakefulness, non-REM sleep showed a global increase in slow-wave activity (636  $\pm$  119% of average waking power, mean  $\pm$  standard

error of the mean; P = 0.004, T = 4.8 paired t-test, n = 5). The topographic distribution of high frontal slow-wave activity (Fig. 1, right) was also near to normal for patients in a minimally conscious state, though some showed lateralization due to massive hemispheric brain lesions. The polysomnography of patients in a minimally conscious state also resembled that of healthy controls with alternating cycles of non-REM and REM sleep, with REM sleep periods progressively increasing in duration at the end of the night (Fig. 2). Finally, the five patients in a minimally conscious state who showed consolidated behavioural sleep showed a statistically significant (P < 0.05) homoeostatic decline of slow-wave activity over the night (Fig. 2).

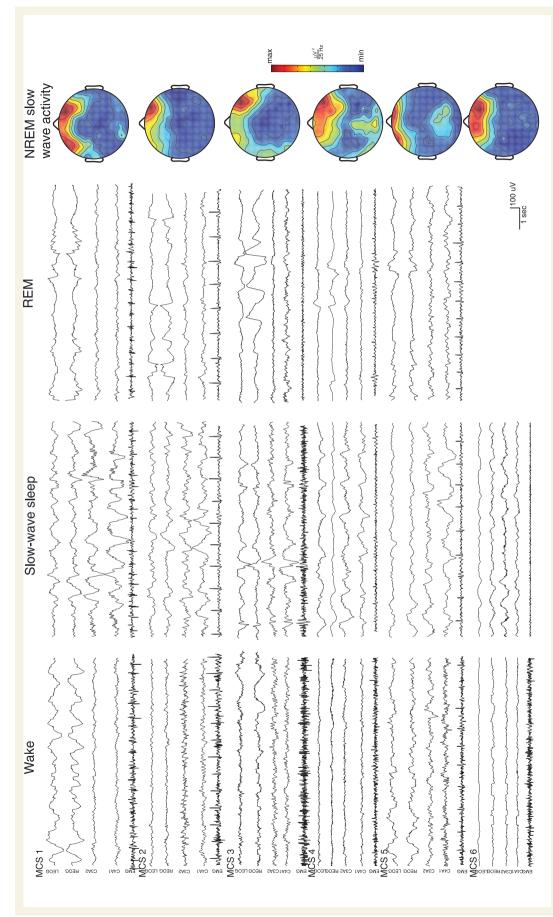
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In contrast, no pattern of normal electrophysiological sleep could be observed in the five patients in a vegetative state (Fig. 3, Table 3). Consistent with the clinical definition of vegetative state, prior to, during and after the study, four out of five vegetative state patients showed a clear behavioural sleep wake cycle, i.e. the alternating of sustained periods of eyes opening, followed by long-lasting eyes-closed periods during the night. One patient (VS4) clinically presented with only intermittent eye opening and very low arousal prior to and during most of the recording. In all patients in a vegetative state, behavioural transition to sleep was not accompanied by clear changes in the EEG (Fig. 3, left). No stages 2-3 of non-REM sleep or REM sleep could be identified and therefore we could only classify the EEG as either 'eyes open' or 'eyes closed.' While most of the patients in a vegetative state did have the characteristic slowing of EEG rhythms in the delta and theta frequency ranges, there was no significant change in slow-wave activity when patients closed their eyes (97  $\pm$  19% of the global average eyes open power, mean  $\pm$ standard error of the mean; P = 0.45, T = -0.15 paired t-test, n = 5). We did not observe sleep spindles in any of the patients in a vegetative state. Polysomnography did not reveal any pattern of sleep cycles and we could not observe a homoeostatic decline of sleep-related slow-wave activity (P > 0.05) during the night in any of the patients in a vegetative state. Figure 4 reports Patients VS1-4. Although they did not correspond to normal sleep, Patient VS5's results were atypical and are described in the Supplementary material.

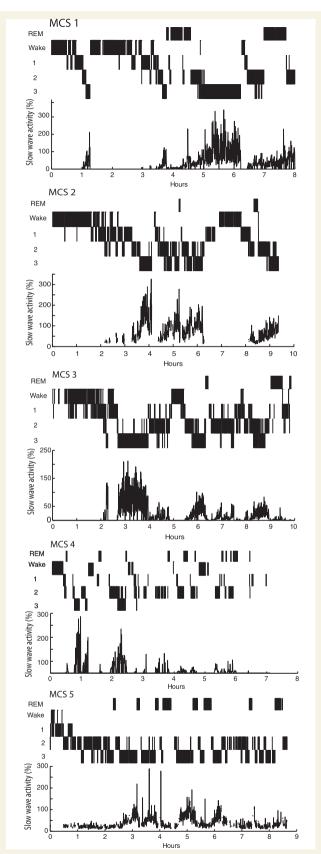
# **Discussion**

# Clinical and neuroscientific relevance of a link between the presence or absence of normal sleep patterns and the level of consciousness

In contrast to patients in a minimally conscious state, none of the patients in a vegetative state showed any electrophysiological features of normal sleep, even if preserved behavioural sleep-wake cycles could be observed in most patients. These results suggest that electrophysiological sleep features observed during the night could possibly be a reliable indicator of the patient's level of consciousness, differentiating patients in a vegetative state from those in a minimally conscious state. Such studies could potentially be a



MCS6, did not have any REM during the recording. Right: Topographic distribution of slow wave activity during non-rapid eye movement (NREM) sleep for the entire night. Colour bars Figure 1 Sleep in six patients in a minimally conscious state. Left: electrooculogram, EEG and EMG 10 s traces for three states: Wake, slow-wave sleep and REM sleep. One subject, represent the average absolute electrographic power (uV2/0.25 Hz frequency bin for the 0.5-4.5 Hz range) expressed as the maximum and minimum power for each individual.



**Figure 2** Homoeostatic decline in slow wave activity of five patients in a minimally conscious state. Hypnogram and slow-wave activity time course. Sleep stages represented as REM, Wake, Stages 1, 2 and 3. The time course of slow-wave

Table 3 Presence or absence of sleep patterns

Subject	Eyes open	Eyes closed	Spindles	Slow waves	REM
MCS 1	+	+	+	+	+
MCS 2	+	+	+	+	+
MCS 3	+	+	+	+	+
MCS 4	+	+	+	+	+
MCS 5	+	+	+	+	+
MCS 6	+	+	+	+	_
VS 1	+	+	_	_	_
VS 2	+	+	_	_	_
VS 3	+	+	_	_	_
VS 4	+	+	_	_	_
VS 5	+	+	_	_	_

useful complement to bedside behavioural assessment in the evaluation of brain function in non-communicative brain-damaged patients.

Failure to show EEG correlates of behavioural changes in vigilance for patients in a vegetative state could have at least two different origins. First, they could be due to insufficient modulation of corticothalamic activity by a deficient ascending reticular activating system. This explanation could prevail in Patient VS4, where the altered state of consciousness was caused by a focal pontine haemorrhage, and in which behavioural sleep-wake cycles were also relatively deficient. Even if transient periods of behavioural wakefulness (increased arousal, eyes open) were observed, no related EEG change could be detected in this patient. On the other hand, the absence of electrophysiological sleep could also be explained by a preserved modulation of activity in the ascending reticular system, but a failure in corticothalamic function to propagate signals from the ascending reticular activating system. Patients in a vegetative state typically show a pattern of widespread thalamocortical dysfunction and metabolic impairment, in particular in frontoparietal cortices (Laureys et al., 2002, 2004). Frontoparietal cortices, including default network areas, have also been involved in the generation of sleep patterns such as slow waves (Dang-Vu et al., 2008; Murphy et al., 2009). Though spindles are thought to involve primarily a thalamic generator, frontoparietal circuits are involved in their propagation (Schabus et al., 2007) and synchronization (Evans, 2003). More generally, widespread functional impairment of thalamocortical circuitry could potentially explain both the impairment of consciousness and the absence of normal sleep electrophysiological features of patients in a vegetative state. These two different mechanisms could lead to a differential prognosis and different therapeutic approaches in individual patients. For example, at the population level, patients with isolated subcortical arousal system function impairment could

#### Figure 2 Continued

activity for a single channel near Fz is expressed as a percentage of the mean slow-wave activity reading for the entire night. MCS = patients in a minimally conscious state.

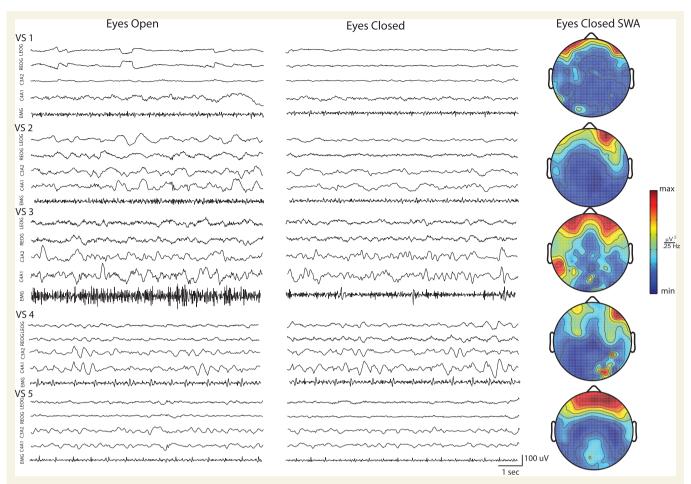


Figure 3 Behavioral sleep patterns for patients in a vegetative state and slow-wave activity topography. (Left) electrooculogram, EEG and EMG 10 s traces for eyes open and eyes closed. (Right) Topographic distribution of the average slow wave activity during the eyes closed condition for the entire night. Colour bars represent the absolute electrographic power (uV2/0.25 Hz frequency bin for the 0.5-4.5 Hz range) expressed as the maximum and minimum power for each individual. SWA = slow-wave activity; VS = patients in a vegetative state.

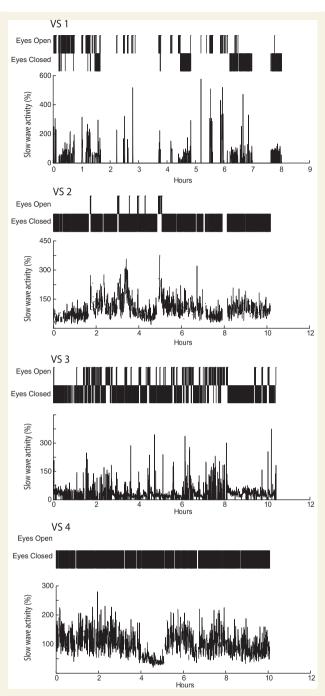
have a better prognosis and would be more likely to respond to central thalamic stimulation or arousal-promoting drugs than patients with more widespread thalamocortical damage. Further studies are needed before a link between polysomnographic EEG patterns and differences in prognosis and response to treatment can be assessed in populations of patients in a vegetative state.

No REM sleep patterns, as defined by wakefulness-like EEG associated with rapid ocular saccades and decreased muscle tone, were observed for patients in a vegetative state. As shown in early experiments in cats, REM sleep generating mechanisms located in the dorsal pontine tegmentum are sufficient to generate periods of atonia accompanied by rapid eye movements (Jouvet, 1972). Brainstem function is typically preserved in patients in a vegetative state (Boly et al., 2008b). Thus, it is possible that brainstem-generated features of REM sleep not involving changes in cortical activity may be present in at least some vegetative patients. A recent study (Bekinschtein et al., 2009b) suggests that circadian rhythmicity may be impaired in patients in a vegetative state, depending on the type of injury and the level of consciousness. In the present study, while we could not rigorously establish

to what extent circadian rhythmicity was preserved, we did observe extended periods of behavioural sleep that occurred more at night than during the day.

In contrast to patients in a vegetative state, subjects in a minimally conscious state showed all stages of sleep. These results suggest a global preservation of brain function in these patients. This observation is in line with previous studies showing preserved response to external stimuli (Boly et al., 2004, 2008a) and large scale brain network connectivity (Vanhaudenhuyse et al., 2010) in minimally conscious patients. The presence of spindles also suggests that patients in a minimally conscious state show a relative preservation of thalamocortical connectivity compared to patients in a vegetative state (Vanhaudenhuyse et al., 2010). The preservation of REM sleep patterns in minimally conscious patients also has some potential clinical relevance. REM sleep has been linked in healthy volunteers to emotional content and vivid visual imagery (Nir and Tononi, 2010) that could also be present in these patients. Further investigations should study residual cognitive function of patients in a minimally conscious state, which, though unable to communicate, seem to have relatively preserved brain function and likely present some capacity for perception and cognition.

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**Figure 4** Hypnogram and slow-wave activity time course in four patients in a vegetative state. Behavioural sleep patterns represented as eyes open and eyes closed. The time course of slow-wave activity for a single channel near Fz is expressed as a percentage of the mean slow-wave activity reading for the entire night.

We also observed that in contrast to patients in a minimally conscious state, patients in a vegetative state did not show detectable sleep cycle architecture and homoeostatic regulation of slow-wave activity. As slow-wave activity has been suggested to be linked to plasticity (Huber *et al.*, 2004; Landsness *et al.*, 2009), our findings could also partially explain the better prognosis observed

in large cohort studies comparing patients in a minimally conscious state to those in a vegetative state (Luaute *et al.*, 2010). However, further studies on larger numbers of patients are required before a link between prognosis and different sleep patterns can be asserted.

It should be stressed that one should remain cautious when interpreting the functional significance of sleep measurements in terms of level of consciousness in brain damaged patients. For now, one cannot exclude that individual patients in a vegetative state could present some partial preservation of sleep electrophysiological features. More investigations during pharmacological manipulations, such as general anaesthesia, in patients with status epilepticus and a larger cohort of patients with pathological alterations of consciousness are also needed before a consensus can be reached on the generalizability of our findings.

# Technical issues in the study of EEG sleep recordings analyses in severely brain damaged patients

Studying polysomnographic recordings in patients with altered states of consciousness represents a major technical and neuroscientific challenge. Special care should be taken while examining EEG traces and analyses should be performed only on artefact free segments. Two patients in a minimally conscious state had to be discarded from our analyses because of excessive noise and artefacts in the recordings. In addition, special care should be taken in the differentiation of patients in minimally conscious and vegetative states and in the use of appropriate behavioural scales. Videotaped recordings are also very helpful as these patients can present fragmented sleep, leading to more difficult interpretation of the findings in the absence of behavioural status. Automatic sleep scoring should be only used with caution, due to the presence of slower baseline EEG in a number of brain damaged patients, as compared to healthy controls. The assessment of alternating sleep stages, as well as quantification of spindles and slow-wave activity topography and homoeostasis were used to illustrate differences between-patient populations. A comparison of slow-wave activity between wake and sleep was performed to provide an additional, quantitative assessment of EEG changes in relation to changes in vigilance. We used a two electrodes system for the sleep scoring due to the well-established tradition of using C3 and C4 (Rechtschaffen and Kales, 1968). All other analysis (homoeostatic decline and topography) took advantage of the high spatial resolution and the larger amount of data provided by high-density EEG. It is likely that most of the findings reported here could have been identified with a smaller number of electrodes, as used in clinical routine. However, high-density EEG recordings allowed us to perform a detailed topographic analysis of sleep patterns in individual subjects, despite the presence of extensive focal brain lesions that are common in these patients. In our case, the use of a large number of electrodes minimized the risk of false negative findings by covering a larger surface of the brain than conventional recordings and by allowing the sampling of isolated functioning brain regions, which are not uncommon in these patients (Schiff et al., 2002). In addition, this technique is

ideally suited to the fine-grained topographic analysis of sleeprelated EEG features such as slow-waves and spindles. Future studies should also investigate scalp propagation and cortical generators of these sleep-related rhythms in individual brain damaged patients. Further studies investigating changes in brain responses to external stimulation of patients in minimally conscious and vegetative states in different behavioural vigilance stages would also provide a useful complement to studies investigating changes in spontaneous EEG.

A remaining question is the relationship between structural and functional brain connectivity preservation and sleep patterns in non-communicative brain-damaged patients. Further multi-modal studies should combine EEG recordings to resting state functional MRI data and structural MRI (e.g. diffusion tensor imaging data) in these patients to better address this question. Further studies should also investigate the relationship between prognosis and fine-grained sleep EEG characteristics of individual patients in minimally conscious or vegetative states.

## Conclusion

We have identified a relationship between the presence of normal sleep electrophysiological features and the level of consciousness in severely brain damaged patients. These results suggest that after further validation, the present methodology could potentially be rapidly translated into a routine clinical setting and bring relevant complementary information on the patients' residual brain function to bear on their clinical evaluation. In addition, assessment of sleep homoeostatic measures such as slow-wave activity could be a useful paraclinical marker of the potential for plasticity in individual patients in a minimally conscious or vegetative state, complementing their bedside and standard prognostic assessment. Future studies on larger samples of patients will aim at correlating electrophysiological sleep features with prognosis and white matter anatomical damage (as assessed for example by diffusion tensor imaging) in these severely brain damaged patients.

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# Supplementary material

Supplementary material is available at Brain online.

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